Available online on 15.09.2026 at <http://jddtonline.info>

Journal of Drug Delivery and Therapeutics

Open Access to Pharmaceutical and Medical Research

Copyright © 2026 The Author(s): This is an open-access article distributed under the terms of the CC BY-NC 4.0 which permits unrestricted use, distribution, and reproduction in any medium for non-commercial use provided the original author and source are credited



Open Access Full Text Article

Review Article

Impact of Nasal Delivery Devices on Olfactory Drug Deposition

Niharika Sahu², Ruchi Gupta¹, Rupesh Sahu³, Rahul Dev¹, Dharmendra Sahu¹, Shiv Kumar Bhardwaj^{3*}

¹ Gracious College of Pharmacy, Village-Belbhata, Abhanpur, Raipur-493661, Chhattisgarh, India

² Columbia College of Pharmacy, Columbia Professional University, Tekari, Near Vidhansabha Road, Raipur-493111, Chhattisgarh, India

³ Columbia Institute of Pharmacy, Columbia Professional University, Tekari, Near Vidhansabha Road, Raipur-493111, Chhattisgarh, India

Article Info:



Article History:

Received 09 June 2026

Reviewed 17 July 2026

Accepted 01 Aug 2026

Published 15 Sep 2026

Cite this article as:

Sahu N, Gupta R, Sahu R, Dev R, Sahu D, Bhardwaj SK, Impact of Nasal Delivery Devices on Olfactory Drug Deposition, Journal of Drug Delivery and Therapeutics. 2026; 16(9):326-334 DOI: <https://doi.org/10.22270/jddt.v16i9.8009>

For Correspondence:

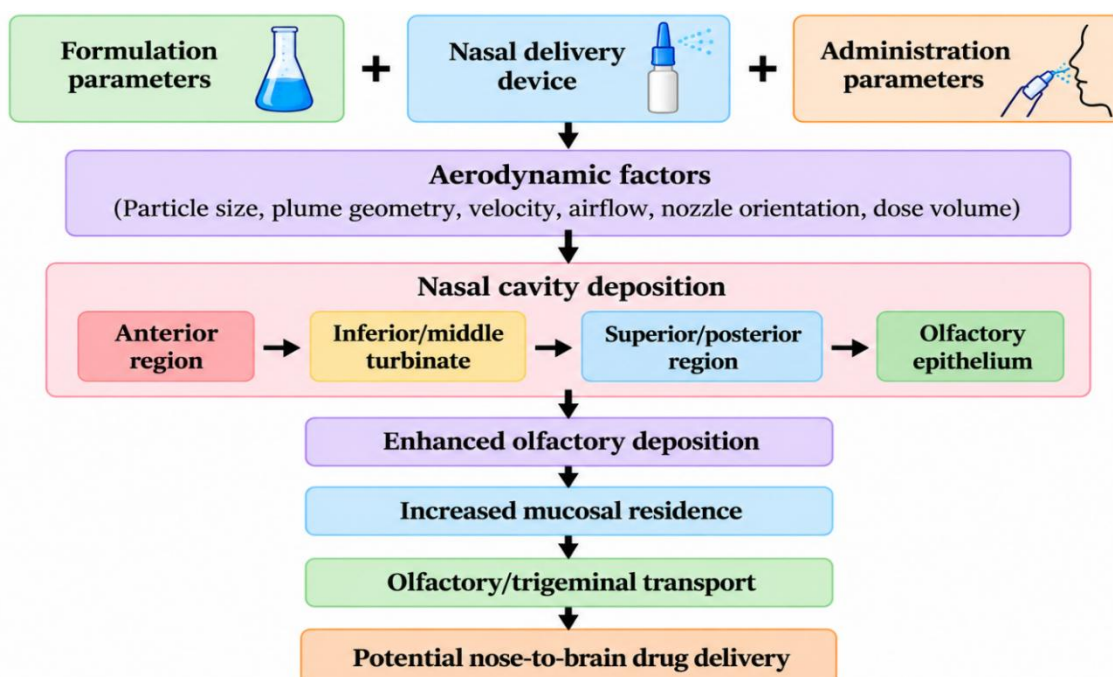
Shiv Kumar Bhardwaj, Columbia Institute of Pharmacy, Columbia Professional University, Tekari, Near Vidhansabha Road, Raipur-493111, Chhattisgarh, India

Abstract

Nasal delivery offers a promising non-invasive approach for targeting therapeutics to the brain through the olfactory region. However, conventional nasal administration frequently produces predominant deposition in the anterior nasal cavity, limiting drug access to the olfactory epithelium. Nasal delivery devices play a critical role in overcoming these anatomical and aerodynamic barriers by controlling spray velocity, droplet or particle size, plume geometry, airflow, dose volume and administration direction. This review examines the impact of conventional and advanced nasal delivery devices on olfactory drug deposition, with particular emphasis on metered-dose sprays, nasal drops, nebulizers, powder devices, atomizers, breath-powered bidirectional systems and specialized nose-to-brain platforms. The influence of device design and administration parameters on regional deposition, mucosal retention and potential nose-to-brain transport is discussed. Computational fluid dynamics, nasal cast models, imaging techniques and experimental approaches used for deposition assessment are also reviewed. Emerging personalized and digitally optimized devices may provide improved and reproducible olfactory targeting for future CNS therapeutics.

Keywords: Olfactory deposition, nasal delivery devices, nose-to-brain delivery, intranasal drug delivery, olfactory targeting

Graphical abstract



Highlights

- ✓ Device parameters influence aerodynamic transport and olfactory deposition.
- ✓ Optimized plume geometry and airflow can reduce anterior nasal impaction.
- ✓ Formulation properties affect aerosolization, deposition and mucosal retention.
- ✓ Patient anatomy and technique influence regional nasal drug deposition.
- ✓ Advanced devices may enhance olfactory targeting and nose-to-brain delivery.

1. Introduction

The nasal route has attracted considerable interest as a non-invasive pathway for delivering drugs to the central nervous system because the olfactory epithelium provides anatomical connectivity with the brain.¹ However, achieving therapeutically meaningful deposition in the olfactory region remains difficult because the nasal valve, turbinates, complex nasal geometry, mucus layer and mucociliary clearance can divert formulations toward the anterior cavity or nasopharynx.² Conventional nasal sprays generally produce greater deposition in the anterior and middle nasal regions, whereas specialized devices attempt to improve delivery toward the superior/posterior nasal cavity.³ Device-related parameters-including nozzle geometry, spray angle, plume width, droplet size, velocity, airflow and administration technique-therefore represent critical determinants of olfactory deposition.⁴ Recent research has increasingly shifted from simply selecting an intranasal formulation toward integrating formulation characteristics with device engineering and patient-specific administration.⁵ Advanced breath-powered, bidirectional, atomization-based and personalized devices offer opportunities for more reproducible olfactory targeting.⁶

2. Nasal anatomy and the olfactory target

The nasal cavity is anatomically organized into the vestibular, respiratory and olfactory regions, with the olfactory epithelium predominantly located in the superior nasal cavity around the olfactory cleft.⁷ This region is an important target for nose-to-brain delivery because its olfactory neurons provide a potential anatomical route toward the central nervous system.⁸ However, achieving selective and efficient olfactory deposition remains challenging because of the nasal

valve, complex turbinate structure, narrow olfactory cleft, limited olfactory surface area, mucociliary clearance, inter-individual anatomical variability, anterior leakage or swallowing and device-dependent aerosol behavior.⁹

3. Device-dependent determinants of olfactory deposition

3.1 Droplet/particle size

Particle or droplet size strongly influences nasal deposition. Very large droplets tend to impact the anterior nasal cavity, whereas smaller particles may penetrate deeper into the nasal passage depending on airflow and aerodynamic characteristics. Human nasal-cast and computational studies have identified particle size and flow conditions as important variables governing olfactory deposition.¹⁰

3.2 Plume geometry

A narrow and appropriately directed plume can improve penetration toward the superior/posterior nasal cavity. Plume angle and spray direction therefore represent important device-design variables.¹¹

3.3 Airflow

Controlled airflow can transport aerosol beyond the nasal valve and improve posterior deposition. Breath-powered bidirectional devices are particularly relevant because exhaled airflow can facilitate movement toward the upper nasal regions while reducing unwanted pulmonary or oropharyngeal delivery.¹²

3.4 Nozzle orientation

Nozzle position and insertion angle affect the trajectory of the emitted formulation. Incorrect orientation can increase anterior deposition and reduce access to the olfactory cleft.¹³

3.5 Administration technique

Head position, breathing pattern, dose volume, nostril selection and administration angle can substantially alter regional deposition. Thus, device performance cannot be considered independently of user technique.¹⁴

Figure 1 illustrates the key factors governing nasal drug deposition and potential nose-to-brain transport, highlighting the influence of device, formulation and patient parameters on aerodynamic transport, olfactory deposition, mucosal retention and subsequent delivery toward the central nervous system.

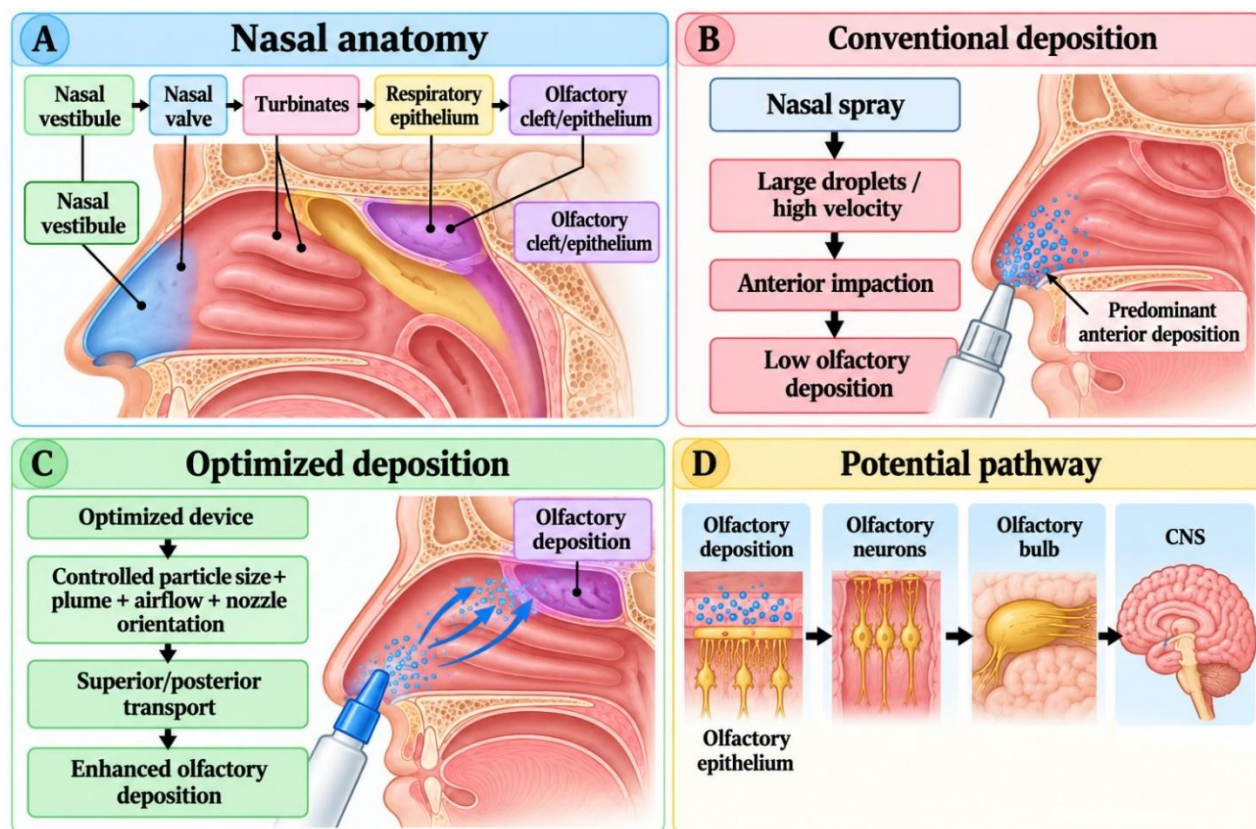


Figure 1. Anatomical and mechanistic basis of olfactory drug deposition

(Schematic illustration of nasal anatomy, conventional versus optimized deposition and the potential pathway of drug transport from the olfactory epithelium to the brain.)

4. Classification of nasal delivery devices

Table 1. Major nasal delivery devices and their deposition characteristics

Device	Primary mechanism	Typical deposition tendency	Olfactory targeting potential	Major limitation	Ref
Nasal drops	Gravity-driven	Variable; highly position dependent	Low-moderate	Runoff and poor dose precision	15
Conventional nasal spray	Mechanical pump	Mainly anterior/middle cavity	Low-moderate	Limited superior deposition	16
Metered-dose spray	Metered aerosol	Anterior/middle regions	Moderate with optimization	Device/formulation dependent	17
Nebulizer	Continuous aerosol generation	Can reach deeper regions	Moderate	Requires appropriate airflow	18
Nasal powder device	Dry-powder dispersion	Depends on particle properties	Moderate-high	Powder deagglomeration	19
Breath-powered device	Patient-generated airflow	Posterior/superior regions	High	Patient cooperation required	20
Bidirectional device	Controlled airflow through nasal cavity	Upper/posterior cavity	High	More complex administration	21
Specialized atomizer	Controlled aerosolization	Optimized regional deposition	High	Cost and device complexity	22
Personalized device	Anatomy-specific delivery	Targeted	Potentially very high	Limited clinical validation	23

5. Impact of conventional nasal devices

Conventional metered-dose nasal sprays are widely used because of their portability, dose reproducibility, ease of administration and rapid drug delivery.²⁴ However, the generated aerosol plume may undergo inertial impaction at the nasal valve and anterior nasal structures, resulting in predominant anterior deposition followed by mucociliary clearance or swallowing and consequently reducing drug exposure to the olfactory

region.²⁵ Therefore, despite their established clinical utility, conventional nasal sprays have limited ability to achieve selective and efficient olfactory targeting.²⁶ **Figure 2** highlights the major device, formulation and patient-related factors that influence aerodynamic drug transport within the nasal cavity, determining whether deposition occurs predominantly in the anterior region or is directed toward the superior/posterior olfactory region, thereby affecting mucosal retention and the potential for nose-to-brain drug transport.

6. Advanced devices for olfactory targeting

Table 2. Advanced device strategies for improving olfactory deposition

Device strategy	Main principle	Expected effect	ReF
Breath-powered delivery	Uses controlled exhalation	Improves posterior/superior transport	27
Bidirectional delivery	Air enters one nostril and exits the other	Enhances upper nasal deposition	28
Vortex aerosolization	Generates controlled aerosol flow	Improves targeting of upper nasal regions	29
Specialized nozzle	Controls direction and plume	Reduces anterior impaction	30
Powder delivery	Optimizes aerodynamic particle behavior	Potentially improves regional penetration	31
Pulsating aerosol	Controls aerosol delivery over time	May improve deposition uniformity	32
Personalized nozzle	Adapted to patient anatomy	Potentially improves reproducibility	33
3D-printed device	Patient-specific geometry	Enables individualized targeting	34

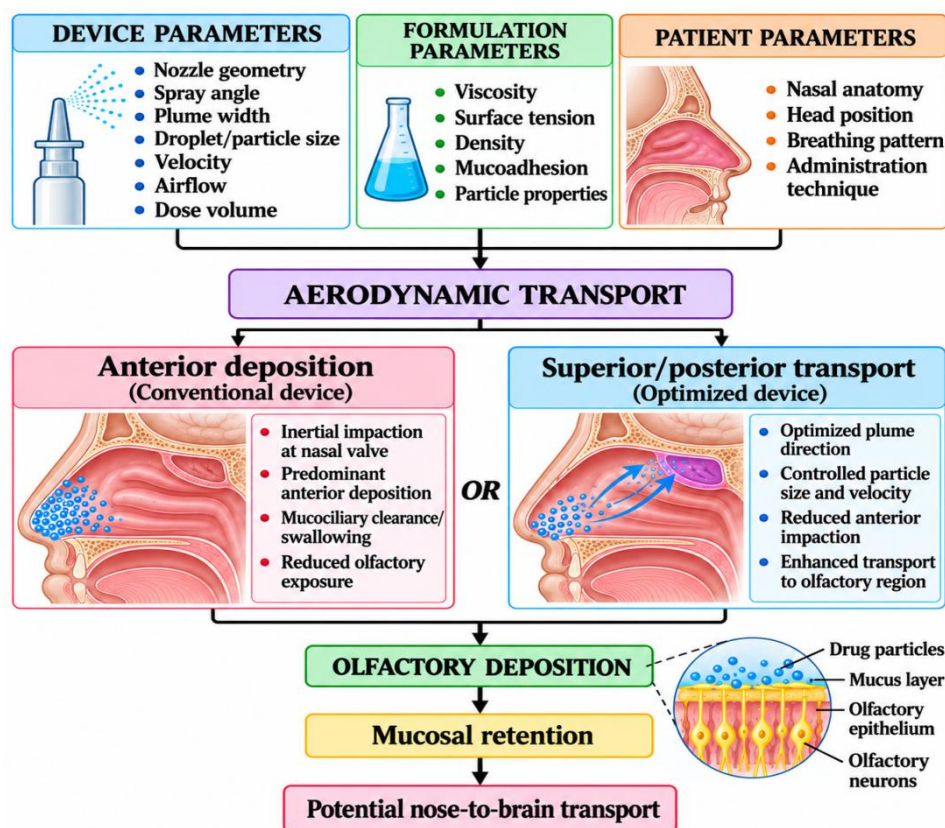


Figure 2. Device-formulation-deposition relationship

(Schematic representation of device, formulation and patient factors influencing aerodynamic transport, olfactory deposition, mucosal retention and potential nose-to-brain delivery).

7. Comparative evaluation of device performance

Table 3. Factors influencing olfactory deposition

Factor	Low/poor condition	Optimized condition	Influence on deposition	ReF
Droplet size	Excessively large	Optimized aerodynamic size	Controls regional impaction	35
Spray velocity	Very high	Controlled	Reduces anterior impaction	36
Plume angle	Broad	Narrow/controlled	Improves targeting	37
Nozzle orientation	Incorrect	Anatomically optimized	Improves olfactory access	38
Airflow	Uncontrolled	Controlled	Enhances posterior transport	39
Dose volume	Excessive	Optimized	Reduces runoff	40
Formulation viscosity	Very low/high	Optimized	Influences retention and spreading	41
Muco-adhesion	Low	Appropriate	Increases residence time	42
Head position	Non-optimized	Appropriate	Alters regional deposition	43
Patient breathing	Normal/uncontrolled	Device-guided	Influences aerosol transport	44

8. Breath-powered and bidirectional delivery

Breath-powered and bidirectional nasal delivery systems are promising approaches for olfactory targeting, as they use controlled airflow rather than relying solely on mechanical spray momentum to transport formulations deeper into the nasal cavity.⁴⁵ Experimental evidence suggests that bidirectional administration can enhance deposition in the upper and

posterior nasal regions compared with conventional unilateral spray delivery, with one study reporting approximately 32% upper-posterior deposition using a bidirectional device compared with 11% using a conventional spray pump.⁴⁶ Thus, these systems may help overcome a key limitation of conventional nasal delivery-insufficient penetration beyond the nasal valve.⁴⁷

9. Computational and experimental assessment

Table 4. Methods for evaluating olfactory drug deposition

Method	Application	Major advantage	Major limitation	ReF
Computational fluid dynamics (CFD)	Predicts airflow and particle trajectories	Non-invasive prediction	Requires validated models	48
Human nasal casts	Regional deposition studies	Anatomically relevant	Cannot fully reproduce physiology	49
Gamma scintigraphy	<i>In vivo</i> regional distribution	Quantitative imaging	Radiation exposure	50
Fluorescence imaging	Deposition visualization	Relatively simple	Mainly experimental	51
MRI/CT-based modeling	Patient-specific anatomy	Individualized modeling	Cost and complexity	52
Laser diffraction	Particle-size analysis	Rapid characterization	Does not directly measure deposition	53
Cascade impaction	Aerodynamic particle size	Detailed aerosol characterization	Laboratory based	54
<i>In vivo</i> pharmacokinetics	Exposure assessment	Biological relevance	Difficult to establish direct brain transport	55

10. Formulation-device interaction

Device optimization alone may not ensure enhanced olfactory deposition, as formulation characteristics-including viscosity, surface tension, density, particle size, muco-adhesion and rheological properties-also influence aerosolization and subsequent nasal

transport.⁵⁶ Therefore, effective olfactory targeting requires coordinated optimization of both formulation and device attributes.⁵⁷ Recent studies combining machine-learning approaches with experimental optimization further suggest that formulation and spray characteristics can be jointly optimized to improve drug deposition in the olfactory region.⁵⁸

Table 5. Formulation-device interactions affecting olfactory deposition

Formulation property	Device parameter	Deposition consequence	Ref.
Viscosity	Spray pressure	Influences atomization	59
Surface tension	Nozzle geometry	Influences droplet formation	60
Particle size	Airflow	Determines aerodynamic transport	61
Density	Spray velocity	Influences inertial behavior	62
Muco-adhesion	Dose volume	Influences retention	63
Rheology	Pump mechanism	Influences plume formation	64
Solid-state properties	Powder device	Influences dispersion	65
Drug concentration	Metering system	Determines delivered dose	66

11. Emerging personalized nasal delivery

A major future direction in olfactory drug delivery is the development of patient-specific nasal delivery systems, as considerable inter-individual variation in nasal anatomy can influence regional drug deposition and may limit the reproducibility of conventional devices.⁶⁷ Recent approaches have explored 3D-printed personalized devices designed to position drug-loaded formulations toward the olfactory region; however, their clinical translation still requires extensive human validation, particularly regarding drug-loading capacity and reproducibility.⁶⁸ In parallel, artificial intelligence (AI) and machine-learning (ML) techniques offer opportunities for individualized optimization by integrating patient anatomy, formulation properties, device parameters and deposition outcomes.⁶⁹ Such data-driven approaches may enable more precise prediction and optimization of olfactory deposition and support the development of anatomy-guided nasal delivery systems. Recent research has also demonstrated the potential of ML-assisted optimization of nasal spray characteristics for improving olfactory-region deposition.⁷⁰

12. Current challenges and future perspectives

A key challenge in evaluating nose-to-brain delivery is that an increase in brain drug concentration does not necessarily confirm direct olfactory transport, because systemically absorbed drug may also reach the brain through the circulation. Therefore, future research should prioritize standardized olfactory-deposition metrics, patient-specific nasal models, validated CFD simulations, device-formulation co-optimization, reproducible administration techniques, long-term nasal safety and human imaging and pharmacokinetic validation. In addition, AI-assisted device optimization and regulatory standardization are needed to improve the reproducibility and clinical translation of advanced nasal delivery systems. Establishing a clear correlation between olfactory deposition and actual CNS exposure will be particularly important for demonstrating therapeutic relevance. Overall, translation remains challenging because laboratory models may not adequately reproduce human nasal anatomy and

physiology, while standardized methods for characterizing regional deposition are still limited.

13. Conclusion

Nasal delivery devices are a critical determinant of olfactory drug deposition and consequently influence the potential effectiveness of nose-to-brain drug delivery. Conventional nasal sprays generally favor anterior deposition, whereas specialized approaches—including breath-powered, bidirectional, atomization-based, powder and personalized devices—can improve transport toward the superior and posterior nasal cavity. Device parameters such as droplet size, plume geometry, spray velocity, nozzle orientation, airflow and dose volume must be optimized together with formulation properties and administration technique. Evidence from nasal-cast studies, CFD modeling, imaging and experimental investigations supports the concept that rational device engineering can substantially improve regional deposition. However, enhanced olfactory deposition should not automatically be interpreted as proof of direct brain delivery. Future progress will depend on patient-specific device design, formulation-device integration, standardized deposition assessment, AI-assisted optimization, and well-designed clinical studies. Thus, the future of olfactory drug delivery is likely to shift from conventional nasal administration toward precision, anatomy-guided and digitally optimized delivery systems.

Abbreviations:

AI : Artificial Intelligence
 BBB : Blood Brain Barrier
 CNS : Central Nervous System
 CFD : Computational Fluid Dynamics
 CT : Computed Tomography
 CNS : Central Nervous System
 CNSD : Central Nervous System Delivery
 DP : Dry Powder
 DPI : Dry Powder Inhaler
 FDA : Food and Drug Administration
 GIT : Gastrointestinal Tract
 HPLC : High-Performance Liquid Chromatography
 IV : Intravenous
 LC-MS/MS : Liquid Chromatography-Tandem Mass Spectrometry

MD : Molecular Dynamics
ML : Machine Learning
MRI : Magnetic Resonance Imaging
N2B : Nose-to-Brain
NDD : Nasal Drug Delivery
NDS : Nasal Delivery System
PK : Pharmacokinetics
PD : Pharmacodynamics
PDE : Partial Differential Equation
PDI : Polydispersity Index
SEM : Scanning Electron Microscopy
TEM : Transmission Electron Microscopy
TGI : Trigeminal–Olfactory Interface
USP : United States Pharmacopeia
3D : Three-Dimensional

Declaration:

Ethics approval and consent to participate:

Ethical approval and informed consent were not applicable to this study because it was a narrative literature review that did not involve any original research involving human participants or animals.

Clinical Trial No:

As this manuscript is a narrative review based exclusively on previously published literature and does not involve any clinical trials, clinical trial registration was not required.

Consent for publication:

Clinical trial registration was not required because this manuscript is based solely on a narrative review of previously published literature and does not involve any clinical trials.

Availability of data and material:

Data availability was not applicable because this manuscript is a narrative review based solely on previously published literature and does not involve the generation or analysis of original datasets.

Funding:

The authors declare that no dedicated financial support was received from any governmental, commercial, or non-profit organization for the preparation of this review.

Declaration of competing interest: The authors declare that there are no conflicts of interest regarding the publication of this manuscript.

Acknowledgements:

The authors sincerely acknowledge the Principals of Columbia Institute of Pharmacy, Columbia Professional University, Raipur, Chhattisgarh, India and Gracious College of Pharmacy, Village Belbhata, Abhanpur, Raipur, Chhattisgarh, India, for their valuable encouragement, support and provision of the necessary infrastructure and library facilities that contributed to the successful completion of this review.

Authorship contribution statement:

Niharika Sahu: Writing -review & editing

Ruchi Gupta: Visualization, schematic design, graphical abstract development and figure illustration.

Rupesh Sahu: Literature review, data curation, validation & manuscript evaluation

Rahul Dev: Manuscript writing, review & editing and critical revision

Dharmendra Sahu: Concept development, methodology & critical review

Shiv Kumar Bhardwaj: Writing, methodology, visualization & final editing

References:

1. Khanfar MS, Alaboud SY, Khalil RW, Darweesh RS. Formulation and Characterization of Amisulpride-Poly (Lactic-Co-Glycolic Acid) Nanoparticles Coated with Chitosan for Intranasal Delivery. *AAPS PharmSciTech*. 2026;27(3):153. doi:10.1208/s12249-026-03405-7 <https://doi.org/10.1208/s12249-026-03405-7> PMID:41872643
2. Zhai Z, Wang W, Wang G, et al. Rationalizing nose-to-brain drug delivery: Machine learning-guided optimization and mechanistic elucidation of olfactory deposition for nasal sprays. *Journal of Controlled Release*. 2026;392:114667. <https://doi.org/10.1016/j.jconrel.2026.114667> PMID:41617015
3. DSouza AA, Kahan M, Yang A, Padmakumar S, Bleier BS, Amiji MM. Formulation considerations in enhancing olfactory mucosal deposition for nose-to-brain drug delivery. *Drug Deliv Transl Res*. 2026;16(8):2552-2577. <https://doi.org/10.1007/s13346-026-02097-7> PMID:41865231 PMCID:PMC13346265
4. Wang H, Zhang Y, Zhang Y, et al. Evaluation of rayleigh jet atomizer for intranasal delivery of lipid nanoparticle-siRNA formulations: stability, deposition, and device performance. *Int J Pharm*. 2025;683:126084. <https://doi.org/10.1016/j.ijpharm.2025.126084> PMID:40819710
5. Sunstrom N, Sunstrom FN. Wearable Devices for Subcutaneous Delivery of Large-Volume Biologics: Design, Use, and Regulatory Perspective. *Biomedical Materials & Devices*. 2026;4(4):4116-4135. <https://doi.org/10.1007/s44174-025-00479-y>
6. Sasaki K, Fukakusa S, Torikai Y, et al. Effective nose-to-brain drug delivery using a combination system targeting the olfactory region in monkeys. *Journal of Controlled Release*. 2023;359:384-399. <https://doi.org/10.1016/j.jconrel.2023.06.005> PMID:37315691
7. Huang WH, Hung YW, Hung W, Lan MY, Yeh CF. Murine model of eosinophilic chronic rhinosinusitis with nasal polyposis inducing neuroinflammation and olfactory dysfunction. *Journal of Allergy and Clinical Immunology*. 2024;154(2):325-339.e3. <https://doi.org/10.1016/j.jaci.2024.02.021> PMID:38494093
8. Mathias K, Petronilho F, Danielski LG. Nose-to-brain axis: mechanistic links between nasal microbiome dysbiosis, neuroinflammation, and brain disorders. *Neuroscience*. 2026;598:19-28. <https://doi.org/10.1016/j.neuroscience.2026.01.039> PMID:41619875
9. Chiang H, Martin HL, Sicard RM, Frank-Ito DO. Olfactory drug delivery with intranasal sprays after nasal midvault reconstruction. *Int J Pharm*. 2023;644:123341. <https://doi.org/10.1016/j.ijpharm.2023.123341> PMID:37611854 PMCID:PMC10621325
10. Peng H, Zhang J, Nie W, et al. Multiscale dynamics of respirable coal dust deposition in Miners' Airways: Effects of respiratory intensity, particle size, and density on pulmonary retention. *Powder Technol*. 2026;468:121569. <https://doi.org/10.1016/j.powtec.2025.121569>

11. Kong X, Wang G, Wei S, et al. Macro-micro spray characteristics of nasal spray: Bridging physicochemical properties to precision olfactory delivery. *Chinese Chemical Letters*. 2026;37(10):112085. <https://doi.org/10.1016/j.ccllet.2025.112085>
12. Seifelnasr A, Si XA, Xi J. Quantitative Investigation of Synthetic Mucus Effects on Spray Deposition in a 3D-Printed SLA Nasal Cavity Model. *Pharm Res*. 2025;42(7):1135-1152. <https://doi.org/10.1007/s11095-025-03886-4> PMID:40562873
13. Wu S, Huang Y, Chen W, et al. Determinants of olfactory cleft targeting in intranasal aerosol delivery: a combined computational and experimental study. *European Archives of Oto-Rhino-Laryngology*. Published online June 6, 2026. <https://doi.org/10.1007/s00405-026-10361-2>
14. Ahmed K, Kumar Dubey M, Kumar A, Dubey S. Artificial intelligence and IoT driven system architecture for municipality waste management in smart cities: A review. *Measurement: Sensors*. 2024;36:101395. <https://doi.org/10.1016/j.measen.2024.101395>
15. Radzio J, Suprewicz Ł, Kuang D, et al. Reversibly-sealable microfluidic platform for multi-molecule gradient delivery to large adherent cell cultures. *Biomed Microdevices*. 2026;28(3):50. <https://doi.org/10.1007/s10544-026-00831-z> PMID:42307820 PMCid:PMC13275633
16. Seifelnasr A, Zare F, Si XA, Xi J. Optimized gravity-driven intranasal drop administration delivers significant doses to the ostiomeatal complex and maxillary sinus. *Drug Deliv Transl Res*. 2024;14(7):1839-1859. <https://doi.org/10.1007/s13346-023-01488-4> PMID:38044376
17. Wang G, Yi H, Kong X, et al. A “three-in-one” nose-to-brain delivery strategy: intranasal vancomycin spray achieves simultaneous clearance of pneumococcal colonization, bacteremia, and meningitis. *Int J Pharm*. 2026;701:127148. <https://doi.org/10.1016/j.ijpharm.2026.127148> PMID:42401303
18. Yan R, Zou C, Yang X, et al. Nebulized inhalation drug delivery: clinical applications and advancements in research. *J Mater Chem B*. 2025;13(3):821-843. <https://doi.org/10.1039/D4TB01938E> PMID:39652178
19. Salgado C, Guénée L, Černý R, Allémann E, Jordan O. Nano wet milled celecoxib extended release microparticles for local management of chronic inflammation. *Int J Pharm*. 2020;589:119783. <https://doi.org/10.1016/j.ijpharm.2020.119783> PMID:32827674
20. Tao Y, Wang Z, Xu H, et al. Moisture-powered memristor with interfacial oxygen migration for power-free reading of multiple memory states. *Nano Energy*. 2020;71:104628. <https://doi.org/10.1016/j.nanoen.2020.104628>
21. Palmer JN, Adappa ND, Chandra RK, et al. Efficacy of EDS-FLU for Chronic Rhinosinusitis: Two Randomized Controlled Trials (ReOpen1 and ReOpen2). *J Allergy Clin Immunol Pract*. 2024;12(4):1049-1061. <https://doi.org/10.1016/j.jaip.2023.12.016> PMID:38244014
22. Yuan CS, Hsu CW, Cheng WH, Huang BY, Jiang Y. Optimizing the droplet size distribution of personal nebulizers to enhance the effectiveness of inhalation using 3D printing technology. *J Drug Deliv Sci Technol*. 2026;115:107667. <https://doi.org/10.1016/j.jddst.2025.107667>
23. Casillas JEJ, Valle LF, Pham J, et al. Advancing Prostate Cancer Treatment: A Review of CT and MR-Guided Online Adaptive Radiotherapy Techniques. *Semin Radiat Oncol*. 2025;35(3):342-352. <https://doi.org/10.1016/j.semradonc.2025.04.007> PMID:40516969
24. Economidou SN, Uddin MdJ, Marques MJ, et al. A novel 3D printed hollow microneedle microelectromechanical system for controlled, personalized transdermal drug delivery. *Addit Manuf*. 2021;38:101815. <https://doi.org/10.1016/j.addma.2020.101815>
25. Lobo S, Xi Z, Das D, Hadzimichalis NM, Creek JA. Intranasal Delivery: Formulation Factors and Insights Into User Experience. *AAPS PharmSciTech*. 2025;26(6):179. <https://doi.org/10.1208/s12249-025-03171-y> PMID:40593387
26. Keller LA, Merkel O, Popp A. Intranasal drug delivery: opportunities and toxicologic challenges during drug development. *Drug Deliv Transl Res*. 2022;12(4):735-757. <https://doi.org/10.1007/s13346-020-00891-5> PMID:33491126 PMCid:PMC7829061
27. Maaz A, Blagbrough IS, De Bank PA. In Vitro Evaluation of Nasal Aerosol Depositions: An Insight for Direct Nose to Brain Drug Delivery. *Pharmaceutics*. 2021;13(7):1079. <https://doi.org/10.3390/pharmaceutics13071079> PMID:34371770 PMCid:PMC8309016
28. Ma R, Sun S, Wang Y, et al. Optimizing topical delivery to the ostiomeatal complex after functional endoscopic sinus surgery using a bidirectional delivery method. *Int J Pharm*. 2025;686:126333. <https://doi.org/10.1016/j.ijpharm.2025.126333> PMID:41187831
29. Wakayama K, Kurihara S, Kurashina Y. Narrow-width surface acoustic wave device-driven olfactory epithelium-targeted intranasal atomization. *Int J Pharm*. 2026;692:126630. <https://doi.org/10.1016/j.ijpharm.2026.126630> PMID:41611042
30. Fong TYA, Thirugnanasampanthar M, Iley T, Parry M, Forbes B. The effect of spray properties and inspiratory flow rate on regional nasal deposition for pressure-swirl versus soft mist devices. *Int J Pharm*. 2026;700:126991. <https://doi.org/10.1016/j.ijpharm.2026.126991> PMID:42208825
31. Cheng D, Pan T, Wang X, et al. An advanced inhalable dry powder, mucus-penetrating aerosol platform: Bridging Andrographolide delivery with clinical translation. *Biomaterials*. 2025;322:123401. <https://doi.org/10.1016/j.biomaterials.2025.123401> PMID:40347852
32. Sosnowski TR, Florkiewicz E, Sosnowski K. Use of process intensification concepts for targeted delivery of inhaled aerosolized medicines. *Chemical Engineering and Processing - Process Intensification*. 2024;203:109902. <https://doi.org/10.1016/j.cep.2024.109902>
33. Cheepu M, Yenumula P, Shanmugam R. Progression in 3D printing families: laser, powder, nozzle-based techniques. In: *Advances in 3D and 4D Printing of Medical Robots and Devices*. Elsevier; 2025:57-73. <https://doi.org/10.1016/B978-0-443-24861-0.00004-6>
34. Pethappachetty P, Kumar B, Govindaraj A, et al. 3D Printing in Personalized Medicine: Revolutionizing Drug Delivery and Healthcare Applications. *Biomedical Materials & Devices*. 2026;4(4):4219-4240. <https://doi.org/10.1007/s44174-025-00514-y>
35. Li L, Relling ME, Islam S, et al. Optimization of nozzle geometry for virtual impaction across more than one decade in particle size. *J Aerosol Sci*. 2025;184:106516. <https://doi.org/10.1016/j.jaerosci.2024.106516>
36. Chaugule V, dos Reis LG, Fletcher DF, Young PM, Traini D, Soria J. A varying-swirl design concept for dry powder inhalers. *J Aerosol Sci*. 2023;171:106162. <https://doi.org/10.1016/j.jaerosci.2023.106162>
37. Weissburg M. Biologically Inspired Chemical Plume Tracking. In: 2026:285-314. https://doi.org/10.1007/978-3-032-11949-0_9
38. Comparative analysis of drug deposition patterns among three commercial nasal spray brands: A computational and experimental study.
39. Warfield-McAlpine P, Fletcher DF, Zhang F, Inthavong K. Increasing airflow ventilation in a nasal maxillary ostium using optimised shape and pulsating flows. *Biomech Model Mechanobiol*. 2025;24(4):1343-1362. <https://doi.org/10.1007/s10237-025-01971-6> PMID:40562978 PMCid:PMC12246003
40. Ghodsi SH, Zahmatkesh Z, Goharian E, Kerachian R, Zhu Z. Optimal design of low impact development practices in response to climate change. *J Hydrol (Amst)*. 2020;580:124266. <https://doi.org/10.1016/j.jhydrol.2019.124266>
41. Jia W, Pang Y, Zhao C, et al. Low drug load, high retention mometasone furoate cream with polyglyceryl – 3 oleate as a

- chemical enhancer: Formulation development, in vivo and in vitro evaluation and molecular mechanisms. *Int J Pharm.* 2024;659:124284. <https://doi.org/10.1016/j.ijpharm.2024.124284> PMID:38810934
42. Bedhafi T, Idoudi S, Alhams AA, et al. Applications of polydopaminic nanomaterials in mucosal drug delivery. *Journal of Controlled Release.* 2023;353:842-849. <https://doi.org/10.1016/j.jconrel.2022.12.037> PMID:36529384
 43. Liu Z, Huang J, Li P, et al. High-precision inkjet 3D printing of curved multi-material structures: Morphology evolution and optimization. *Addit Manuf.* 2024;94:104497. <https://doi.org/10.1016/j.addma.2024.104497>
 44. Candeloro BM, Oliveira NS, Franchi AC, et al. Systematic Review and Meta-analysis to Investigate the Effects of Cannabidiol on Blood Pressure: Examination of Randomized Triple- and Double-Blind Placebo Trials. *Revista Brasileira de Farmacognosia.* 2025;35(5):878-893. <https://doi.org/10.1007/s43450-025-00680-6>
 45. Sinatra ST., Houston MC. *Nutritional and Integrative Strategies in Cardiovascular Medicine.* CRC Press; 2022. <https://doi.org/10.1201/9781003137849>
 46. Bi-directional nasal drug delivery systems: A scoping review of nasal particle deposition patterns and clinical application.
 47. Gallina A, Gallina M, Cona A, Vitulo P, Mularoni A, Provenzano A. Phage Therapy at the Crossroads Between Clinical Promise and Regulatory Challenge. *Pharmaceuticals.* 2026;19(1):162. <https://doi.org/10.3390/ph19010162> PMID:41599759 PMCID:PMC12845414
 48. Salmanipour S, Salmani Pour Avval S, Inthavong K, Hamishehkar H. Numerical Investigation to Improve Pulmonary Drug Delivery via Dry Powder Inhalers: A Review of In-Silico Modeling. *Pharm Res.* 2025;42(8):1251-1283. <https://doi.org/10.1007/s11095-025-03906-3> PMID:40813932
 49. Silva AC. Current Clinical Evidence on Nose-to-Brain Drug Delivery. *Drug Discov Today.* 2026;31(5):104765. <https://doi.org/10.1016/j.drudis.2026.104765> PMID:42580438
 50. Bailey DL, Hennessy TM, Willows KP, et al. In vivo quantification of ¹⁷⁷Lu with planar whole-body and SPECT/CT gamma camera imaging. *EJNMMI Phys.* 2015;2(1):20. <https://doi.org/10.1186/s40658-015-0123-2> PMID:26501821 PMCID:PMC4573647
 51. D'Angelo D, Kooij S, Verhoeven F, Sonvico F, van Rijn C. Fluorescence-enabled evaluation of nasal tract deposition and coverage of pharmaceutical formulations in a silicone nasal cast using an innovative spray device. *J Adv Res.* 2023;44:227-232. <https://doi.org/10.1016/j.jare.2022.04.011> PMID:36725192
 52. Zhang J, Hu Y, Qin H, et al. Flexible skull-conformal phased array for aberration-corrected transcranial focused ultrasound therapy. *Ultrasonics.* 2026;165:108089. <https://doi.org/10.1016/j.ultras.2026.108089> PMID:41936163
 53. Doub WH, Suman JM, Copley M, Goodey AP, Hosseini S, Mitchell JP. Laboratory Performance Testing of Aqueous Nasal Inhalation Products for Droplet/Particle Size Distribution: an Assessment from the International Pharmaceutical Aerosol Consortium on Regulation and Science (IPAC-RS). *AAPS PharmSciTech.* 2023;24(7):208. <https://doi.org/10.1208/s12249-023-02665-x> PMID:37817001
 54. Nannu Shankar S, Vass WB, Lednický JA, et al. The BioCascade-VIVAS system for collection and delivery of virus-laden size-fractionated airborne particles. *J Aerosol Sci.* 2024;175:106263. <https://doi.org/10.1016/j.jaerosci.2023.106263> PMID:38680161 PMCID:PMC11044810
 55. Yang T, Bai S. In Vitro to In Vivo Extrapolation for Drug Delivery to the Brain. *Curr Pharmacol Rep.* 2025;11(1):56. <https://doi.org/10.1007/s40495-025-00437-8>
 56. Gholizadeh H, Cheng S, Kourmatzis A, et al. In vitro interactions of aerosol formulations with human nasal epithelium using real-time monitoring of drug transport in a nasal mucosa-on-a-chip. *Biosens*
 - Bioelectron.* 2023;223:115010. <https://doi.org/10.1016/j.bios.2022.115010> PMID:36586150
 57. Jain H, Prabhakar B, Shende P. Modulation of olfactory area for effective transportation of actives in CNS disorders. *J Drug Deliv Sci Technol.* 2022;68:103091. <https://doi.org/10.1016/j.jddst.2021.103091>
 58. Zhang Y, Zhang Z, Zhang X, et al. Machine learning guided design and ablation behavior of ZrC-TaC-SiC ternary coatings. *Corros Sci.* 2026;260:113499. <https://doi.org/10.1016/j.corsci.2025.113499>
 59. Camacho-Lie M, Antonio-Gutiérrez O, López-Díaz AS, López-Malo A, Ramírez-Corona N. Factors influencing droplet size in pneumatic and ultrasonic atomization and its application in food processing. *Discover Food.* 2023;3(1):23. <https://doi.org/10.1007/s44187-023-00065-5>
 60. Hernández-Cid D, Pérez-González VH, Gallo-Villanueva RC, González-Valdez J, Mata-Gómez MA. Modeling droplet formation in microfluidic flow-focusing devices using the two-phases level set method. *Mater Today Proc.* 2022;48:30-40. <https://doi.org/10.1016/j.matpr.2020.09.417>
 61. Ciloglu D. The airflow and the regional particle behavior in a human airway under the circulatory breathing conditions: A numerical study. *J Drug Deliv Sci Technol.* 2024;99:105978. <https://doi.org/10.1016/j.jddst.2024.105978>
 62. Godasie SH, Kamali H. Water jet angle prediction in supersonic crossflows: Euler-Lagrange and machine learning approaches. *The European Physical Journal Plus.* 2024;139(3):251. <https://doi.org/10.1140/epjp/s13360-024-05047-9>
 63. Samadian H, Kakaei N, Karami M, et al. Multi-effect formulation based on pH-Responsive psyllium Mucilage/Poly(vinyl alcohol) nanofibers for controlled delivery of mesalamine. *J Drug Deliv Sci Technol.* 2024;92:105348. <https://doi.org/10.1016/j.jddst.2024.105348>
 64. Samadian H, Kakaei N, Karami M, et al. Multi-effect formulation based on pH-Responsive psyllium Mucilage/Poly(vinyl alcohol) nanofibers for controlled delivery of mesalamine. *J Drug Deliv Sci Technol.* 2024;92:105348. <https://doi.org/10.1016/j.jddst.2024.105348>
 65. Xu Y, Harinck L, Lokras AG, et al. Leucine improves the aerosol performance of dry powder inhaler formulations of siRNA-loaded nanoparticles. *Int J Pharm.* 2022;621:121758. <https://doi.org/10.1016/j.ijpharm.2022.121758> PMID:35483619
 66. Haughney J, Lee AJ, McKnight E, Pertsovskaya I, O'Driscoll M, Usmani OS. Peak Inspiratory Flow Measured at Different Inhaler Resistances in Patients with Asthma. *J Allergy Clin Immunol Pract.* 2021;9(2):890-896. <https://doi.org/10.1016/j.jaip.2020.09.026> PMID:33011302
 67. Hejazi M, Alshammari AM, Edwards DJ, Golshahi L. Development of a predictive model for pediatric intranasal drug delivery with nasal sprays: Leveraging intersubject variability in anatomical dimensions, administration-related parameters, and airway patency. *Comput Biol Med.* 2025;187:109746. <https://doi.org/10.1016/j.compbiomed.2025.109746> PMID:39879885 PMCID:PMC12435185
 68. Rajendran J, Esfandyarpour R. Revolutionizing Personalized Health: The Frontier of Wearable Biomolecule Sensors Through 3D Printing Innovation. *Biomedical Materials & Devices.* 2025;3(2):818-834. <https://doi.org/10.1007/s44174-024-00226-9>
 69. Agarwal B, Gaware S, More N, Shinde R, Shivakumar HN, Jagdale S. A review exploring the translational perspective of artificial intelligence in drug discovery and formulation development. *Ann Pharm Fr.* 2026;84(4):559-594. <https://doi.org/10.1016/j.pharma.2026.01.007> PMID:41653969
 70. Karthikeyan S, Raja S, Balasubramanian V, Rusho MA, Shankar K V. Integrating Machine Learning Approach into Plasma-Sprayed Lanthanum Zirconate Coatings for Thermal Barrier Applications. *Journal of Thermal Spray Technology.* 2026;35(4):955-979. <https://doi.org/10.1007/s11666-026-02163-z>