

Available online on 15.09.2021 at <http://jddtonline.info>

Journal of Drug Delivery and Therapeutics

Open Access to Pharmaceutical and Medical Research

Copyright © 2021 The Author(s): This is an open-access article distributed under the terms of the CC BY-NC 4.0 which permits unrestricted use, distribution, and reproduction in any medium for non-commercial use provided the original author and source are credited



Open Access Full Text Article



Review Article

Dry-Coating of Powder Particles is Current Trend in Pharmaceutical Field

Saikh Mohammed Athar Alli

Department of Pharmaceutics, Jeypore College of Pharmacy, Jeypore, Koraput, Odisha, India, 764 005

Article Info:



Article History:

Received 18 August 2021
Reviewed 29 August 2021
Accepted 04 September 2021
Published 15 September 2021

Cite this article as:

Saikh MAA, Dry-Coating of Powder Particles is Current Trend in Pharmaceutical Field, Journal of Drug Delivery and Therapeutics. 2021; 11(5):145-157

DOI: <http://dx.doi.org/10.22270/jddt.v11i5.5034>

*Address for Correspondence:

Professor (Dr.) Saikh Mohammed Athar Alli, Department of Pharmaceutics, Jeypore College of Pharmacy, Jeypore, Koraput, Odisha, India, 764 005.

Abstract

Modification of surface attributes of particles, usually accomplished by coating, is desirable to enhance and maintain their usability. Coating is a multi-step process involving application of the coating material (CoM) onto the substrate, herein powder particles, where the process along with device/ equipment monitors surface attributes of the applied coating. Nowadays competitive market calls for cost cutting to survive product(s). Thus saving of energy and time, minimising number and quantity of additives, reducing and shortening process steps; consequently minimising the coating process cost are main goals while developing coating process for powder particle. Innovation of processes for dry-powder coating (DPC) along with their further development and refinement finds solution to said issues. Further, DPC process does not call for liquid solvent or solution thus are viewed as cost-effective and environmentally safe, DPC process uses thermo-mechanical methods like mechanofusion, magnetic assisted impaction coating (MAIC), hybridization, rotating fluid-bed process, theta-composer, hot-melt coating (HMC), and many others. Besides these available are non-thermo-mechanical methods namely electrostatic coating; supercritical fluids (SCF) based methods like rapid expansion of supercritical fluid (RESF), gas anti-solvent (GAS), SCF anti-solvent, gas-saturated solution (GSS); vapour coating; and others. Basing on said thermo-mechanical and non-thermo-mechanical principle several DPC methods/ process had been reported in scientific literatures and patents. Said DPC method finds multidisciplinary applications like drug delivery and drug development. Diverse devices are there for the DPC process; their method of working, principle, limitations and benefits along with their applicability in pharmaceutical field are discussed and presented in this article.

Keywords: Dry, particle, coating, pharmaceutical, process

INTRODUCTION

Aqueous dispersions based coating process are energy and time consuming reasoning from the low level of the film former (i.e., coating polymer) and large quantity of aqua that calls for evaporation¹⁻⁷.

Issues like cost and regulatory restrictions on use of volatile organic solvents, and energy and time requirement of aqua-solvent based coating process had led to developing specialised dry-coating techniques, over few decades⁴⁻¹². These processes/ techniques find applicability in the coating of the dry powder particles^{2,4,8,9}.

Rational for coating of the dry powder particle are^{4,11,12}:

- To have functional coating that is to modify drug release profile (enteric coating, delayed/ sustained/ extended release coating)^{4,8}.
- For improving aesthetic property (like improvement in appearance, improve product appeal by masking obnoxious taste and odour, facilitate identification and swallowing, and many others)^{4,9},
- To protect degradation of the product and the core from atmospheric degradants like oxygen, light, humidity, etc^{4,10}.

- For facilitating product handling and production, by reducing friction and making them amenable to high-speed packaging equipment^{4,11}.
- To separate incompatible components by coating them individually and separately^{4,12}.

DRY COATING OF POWDER PARTICLES

Coating of powder particle following dry coating technique, a solventless coating process, is followed to have new-generation materials, as the method enables combining powders with different chemical and physical properties to get composites that bears new functionality or improves characteristics of the component materials²⁻⁴. DPC technologies involve mechanically fixing the CoM herein termed guest particle (GP), in fine submicron state, onto surface of the substrate herein termed host particles (HP), relatively larger particles with size 1 to 200 μm ^{2,4}. Here in these coating processes HPs termed cores that are mechanically coated with GPs using no liquid in any forms like binders, solvents, even water^{3,4}.

Advantages

DPC processes/ techniques have follow advantages.

- Aqua and non-aqua solvent is not needed for coating the powder particles^{2,4}.

- Comparing solvent based coating, the dry coating method is less time consuming, environmental friendly, safe and cost-effective^{3,4}.
- A suitable coating methodology for coating drugs and foods those are sensitive to aqua and non-aqua solvents^{3,4}.
- The process does not call for solvent recovery, as required with process based on volatile organic solvent, as are environmental pollutants^{2,4}.
- Said coating processes is rapid that to based on aqueous dispersions, as the later are energy and time consuming arousing out from the lower concentration of film former and large quantity of water that needs evaporation^{2,4}.

Mechanism

From a mechanistic perspective, DPC processes comprises of sequential steps similar to that of conventional solvent-based coatings²⁻⁴. The process begins with pretreatment of CoM followed by application of CoM onto powdery substrate, and relying on adhesive nature of formulation for maintaining coating uniformity during process of film formation²⁻⁴. Follows are summary on mechanisms of film formation in DPC process, while Figure-1 is schematic presentation of the same.

- Layering is of coating powder onto the surface of powder substrate^{2,3}.
- Coalescence & sintering of CoM's particles is bearing through partial fusion of polymer^{3,4}.
- Levelling of CoM includes densification of layer by reduction of empty spaces & smoothing of surfaces^{2,4}.
- Cooling of applied coating layer followed by curing of the coating film²⁻⁴.

In nutshell, film formation occurs by a sequential process involving powder application, coalescence, and sintering.

CLASSIFICATION OF DPC PROCESS/ TECHNOLOGIES

Follows are the classes of DPC process/technologies²⁻⁴.

- Electrostatic coating
 - Corona charging
 - Tribocharging
 - Electrostatic fluidised-bed coating
- MAIC process/technology
- HMC processes/ technologies
 - HMC using tablet coating pan
 - Spray congealing
 - HMC using fluid-bed processor
 - Solid dispersion hot-melt fluid bed coating or tumbling HMC
 - Turbo jet coating process (modified)
 - Theta-composer
 - Mechanofusion
 - HMC using spheronizer
 - Spheroidization
 - Hybridizer

- Vapour coating
 - Chemical vapour deposition (CVD).
 - Plasma enhanced chemical vapour deposition.
 - Initiated chemical vapour deposition.
 - Atomic/molecular layer deposition (ALMD).
 - Fluidised-bed chemical vapour coating
- SCF based coating
 - RESF method
 - GAS process
 - SCF anti-solvent method
 - GSS method

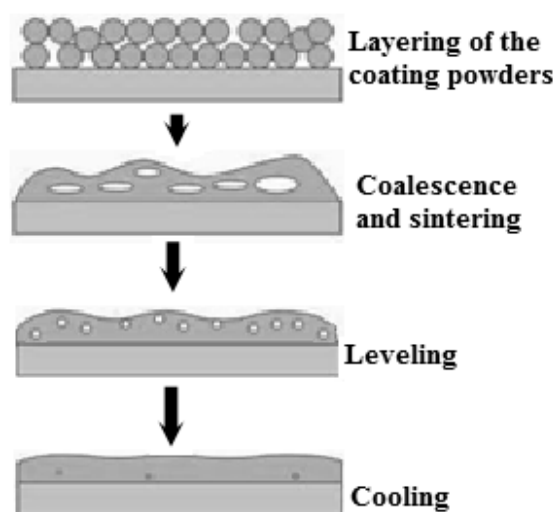


Figure 1: Schematic presentation on principle of DPC²⁻⁴.

ELECTROSTATIC COATING

Electrostatic dry coating, a novel technique, as an alternate to coating processes based on aqueous and non-aqueous solvents finds applicability in pharmaceutical field, besides food and paint technology, metal coatings, and many others^{2, 8, 10}. In pharmaceutical field it is useful technology for coating of powders, tablets, capsules, and living cells^{3, 8, 10}. The method is devised by Yang *et al*^{8, 11, 13, 14} results electrostatic deposition of charged coating particles onto substrate surface, which in turn dramatically enhances uniformity of film coating^{4, 15}. An optimised electrostatic coating process for substrates coating in pan coater can produce coated substrate with excellent coating uniformity, continuous film coat with smooth surface, and drug release significantly similar to that of substrate cores^{2, 8, 15}.

Advantages

Electrostatic dry coating finds advantages as follows^{3, 4, 15}:

- The method is efficient for applying coating solution onto conductive substrates^{2,3}.
- Involves applying strong electrostatic charge onto the substrate^{4,9}.
- CoM comprising oppositely charged conductive ions are sprayed on charged substrates^{3,9}.
- The process makes achievable the uniform and complete coating even of edges and corners^{2,9}.

Principle

Principle of electrostatic coating comprises spraying the mixture of finely grounded polymers and particles onto substrate surface using no any solvent followed by heating of substrate in an oven for curing until powder mixture fuses into film^{2, 4, 8, 10, 15}. Accordingly, the process consists of follow two steps^{3, 8, 15},

- Deposition of the coating particle, and
- Film formation.

The deposition of coating particle step involves spraying of coating powder, onto substrate surface using electrostatic

spray gun, till adequate deposition of coating powder is achieved^{8, 16}. Following coating particle deposition step, there is film formation (curing) step that results coalesce together of the lodged coating particles to form continuous film of coating^{8, 17}. Refer Figure-2 for principle of the electrostatic coating.

Thus the coating assembly comprises of an electrically earthen coating pan, charging gun, and heating source^{8, 15, 18}. Liquid plasticiser spray gun normally is also needed to apply plasticisers^{8, 15}.

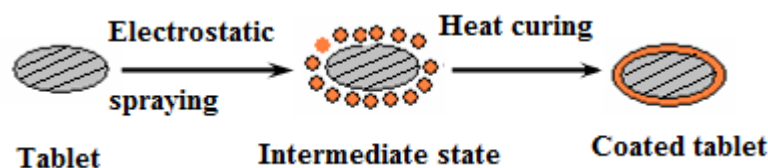


Figure 2: Schematic diagram on principle of electrostatic dry coating²⁻⁴.

The coating process can be promoting by spraying suitable quantity of liquid plasticiser, that is capable of increasing electrical conductivity of substrate and reducing glass transition temperature (T_g) of coating polymer^{8, 15, 17, 19}. Incorporation of plasticiser promotes adhesion of coating particles and film formation, under lower curing temperature, thereby shortens processing time^{15, 20}.

Charging Mechanisms

Basing on charging mechanism, there are two kinds of charging (spraying) units^{9, 15}:

- Corona charging.
- Tribocharging.

Mechanism of corona charging

Said charging mechanism involves electrical breakdown followed by ionising the air by imposing high voltage on charging pins, comprises sharp pointed needle like electrodes, at outlet of gun^{2, 9, 15}. The powdery particles of CoMs pick up negative ions on their passage from gun to substrate^{3, 9, 10}.

Electrical field between earthen substrate and spray gun's charging tip, and repulsive forces amongst charged coating particles generates electrical forces^{4, 9, 10}. Ionisation of the air generates a mechanical force that blows powder towards substrate from charging gun^{2, 9, 10}. Combination of mechanical and electrical forces is resulting movement of particles between substrate and spray gun^{3, 9, 10}. Adjustment of electrical field is done to direct powder flow and control flow pattern, shape, size, and density of powder as it gets released from charging gun^{4, 9, 10}.

Mechanism of tribocharging

Tribocharging mechanism follows principle of friction charging, as of corona charging guns, linked to dielectric

properties of solid materials, thus no electrical field and free ions will be there between spray gun and earthen substrates^{2, 9, 15}. With tribocharging guns, the electrical forces are regarded only from repulsive forces amongst charged particles^{3, 9, 10, 15}. Upon spraying charged particles moves into space adjacent to substrate, and attractive forces between charged particles & earthen substrate make charged particles to deposit on substrate surface^{4, 9, 10, 15}. By virtue of electrostatic attraction and mechanical forces charged particles gets sprayed uniformly onto earthen substrate^{2, 9, 10, 15}.

Charged particles accumulates on substrate surface till repulsive force between particles deposited on substrate surface and approaching particles increases and exceeds electrostatic attraction between the approaching particles and earthen substrate^{3, 9, 15}. Once said repulsive forces gets equivalent to said attractive forces, charged particles no more adheres to substrate surface, thus coating thickness will increase no anymore^{4, 10, 15}.

Limitations

It is more difficult to have electrostatic coating of the electrically non-conducting substrate cores^{10, 15}. For secure smooth and even coating of tablet, powdery organic CoMs must be transmuted into a film with no damage of substrate cores, a difficult task^{10, 15}. Diverse factors like chemical composition of coating solution; hygroscopicity; particle shape, size, and size distribution; corona charging and tribocharging characteristics (i.e., distance and nozzle geometry); electrical resistivity; and many others contributes significantly to coating attributes like adhesion, film thickness, transfer efficiency, and appearance^{10, 15}.

Important patents on coating compositions and apparatus design used for having electrostatic coating of powdery particles onto pharmaceutical dosage forms presented with Table-1^{9, 10}.

Table 1: Important patents on electrostatic coating ^{10, 15}.

Patent number	Publication date	Title of patent	Assignee
GB 2333474 A WO 1998020861 US 20020197388	28-07-1999 22-05-1998 26-12-2006	Method and apparatus for the coating of substrates for pharmaceutical use.	Phoqus Pharmaceuticals Limited, USA.
US 20080020147 US 20070028790 US 20070240976	24-01-2008 08-02-2007 18-10-2007	Method and Apparatus for the Application of Powder Material to Substrates.	Phoqus Pharmaceuticals Limited, USA.
US 7008668B2 CA 2220506A1	07-03-2006 08-01-2008	Powder coating composition for electrostatic coating of pharmaceutical substrates.	Phoqus Pharmaceuticals Limited, USA.
US 20030113445	23-10-2007	Powder material for electrostatic application to a substrate and electrostatic application of the powder material to a substrate.	Phoqus Pharmaceuticals Limited, USA.
WO 1998058748A1	30-12-1998	Electrostatic powder coating of electrically non-conducting substrates.	Raytheon Company, CA, USA
US 20040052938	10-01-2008	Electrostatic application of powder material to solid dosage forms in an electric field.	Phoqus Pharmaceuticals Limited, USA.
WO 2005105317A2 WO 2005105317A3	10-11-2005 16-02-2006	Electrostatic application of powder material to solid dosage forms.	Phoqus Pharmaceuticals Limited, USA.

Electrostatic Fluidised-Bed Coating

In this process powder material kept fluidised in fluidised-bed processor by passing dry air through porous base plate ^{4, 21}. The particles of fluidised powder are subjected for electrical field by either of two ways. One is by of placing an electrode beneath surface of fluidising powder and second is through charge transfer from pre-ionised fluidising air ^{4, 15, 21}. Fluidising effect in addition to repulsive effect of charged powder particles results upward motion of particles; thereby forming cloud of charged particles above the bed ^{20, 21}. Generated cloud is much alike that from conventional electrostatic gun ^{19, 21}. Through the said cloud heated or unheated particle makes several pass ^{4, 16}. Fluidised-bed coating process assisted with electrostatic field never dips the particles into powder bed and generally results thin coat comparing to that from conventional fluidised-bed coating processes ^{4, 16}. Elongated substrates or other objects passing vertically or axially across through powder-bed and through powder cloud gets deposited as layer of powder material, are unsuitable ⁴.

MAIC PROCESS/ TECHNOLOGY

Available diverse DPC process (like compression coating, electrostatic coating, plasticiser dry coating, and heat dry coating); generally involve application of higher impaction force, higher temperature, or high shearing stress to achieve coating ^{9, 22-24}. Strong mechanical force accompanied with generated heat is causes layering and embedding of the GPs (i.e., CoM) onto surface of HPs (substrate cores) ^{10, 22, 23}.

Many pharmaceutical and food ingredients are very heat-sensitive, thermolabile, relatively soft, and easily deformable by intense mechanical and thermal stress ^{9, 10, 24}. These call for soft coating processes/ methods which can attach GPs on HPs with a minimal deformation of particle shape & size, degradation of components by generated heat ^{9, 10}. The MAIC process is developed to solve said issue ²⁻⁴.

Coating of particles onto particles by MAIC involves peening process ²⁻⁴. The process involves pouring small coating particle herein termed GPs and large core particle herein termed HPs into an assembly containing small oscillating magnets ²⁻⁴. Due to oscillation of magnets the small HPs readily gets coated onto GPs ^{2-4, 24}. The process has ability to coat core particle as fine as 0.25 microns. A batch process with shorter processing time demands lower energy ^{4, 24}. For overcoming batch processing limitation of earlier design, continuous type MAIC device is patented that enables separation of coated substrates from magnetic elements for continuous operation ^{2, 3}. Said technique, a soft coating process, developed by Aveka, a US based company, accordingly patented MAIC continuous process to coat small dry particles onto large dry particles ^{3, 4, 9}.

MAIC devices can conveniently handle soft organic GPs and HPs, while coating, without deformation in their particle size and shape ^{2, 10, 24}. This technique can fix GPs onto HPs that are soft with minimal degradation of components and deformation of their particle shape & size ^{2, 4, 10}. Although due to collision of the particles heat is generated, on a micro-scale, during MAIC process is negligible ^{3, 9, 10}. This could be an added advantage while handling thermolabile powders ^{2, 9, 10}.

The process can improve effectiveness of powder's mixing with particles of nano size without aid of heat or solvent ^{3, 25}. Generally, uniform mixing of materials with nano size is more difficult comparing mixing of materials with larger sized particles ^{2, 4, 10}. Still MAIC technology is in development that will be aiding manufacturing applications to produce products with higher quality ^{2, 10}.

Mechanism and Stages of Coating in MAIC Process

During MAIC process, mixture of particles (magnetic particles, GPs, and HPs) stays in fluidised state; where distribution of velocities are Maxwell-Boltzmann type ^{10, 24}.

²⁵. The collision occurring among particles is important to impinge GPs onto surface of HPs and thus formation of semi-permanent coating on surface of substrate, i.e., HPs ^{10,25}. For convenience, the coating mechanism of MAIC processes can be presented as comprising of follow stages, refer Figure-3 ^{2-4,10}.

Stage-1: Excitation of the magnetic particles ^{2,10},

Stage-2: De-agglomeration of the CoM, i.e., GPs ^{3,10},

Stage-3: Spreading and shearing of GPs onto surface of the substrate particles (i.e., particles to be coated or HPs) ^{4,10},

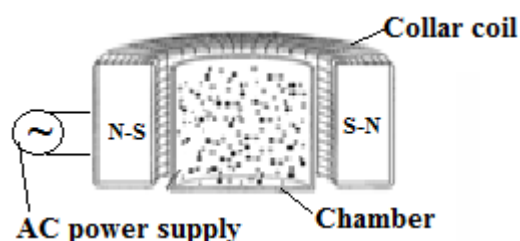
Stage-4: HP-magnetic particle and HP-HP interaction ^{2,10},

Stage-5: Magnetic particle-HP-wall interaction ^{3,10}, and

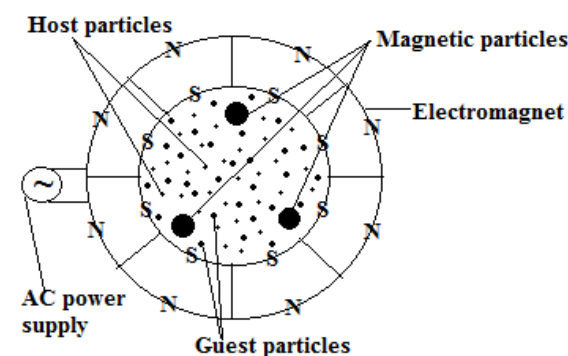
Stage-VI: Formation of products, i.e., coated particles ^{4,10}.

MAIC Apparatus

MAIC apparatus comprises processing vessel that surrounded with series of electromagnets which are



A-Longitudinal section



B-Transverse section

Figure 3: MAIC apparatus. ^{2-4,10}.

Performance of MAIC process depends on parameters like particle size of GPs and HPs, particle size ratio of guest-to-host and magnetic particle-to-HP, ratio of powder mass-to-magnetic particles, processing time, voltage or current and frequency of alternating current, speed of magnetic particle, and many others ^{10, 24-26}. These parameters must be considered during the MAIC process ^{2-4,10}.

However, the coating time depends on several parameters that include number density of HPs, diameter ratio of host-to-guest particles, initial & final bed height of fluidised particle bed, and material properties of GPs and HPs ²³⁻²⁶. There an optimum value of bed-height for which time of coating is minimal ^{10, 25}. Coating time sharply increases as bed-height is lower or higher than optimal value, and/or as diameter of the HPs increases and/or ratio of diameter for host-to-guest particle is increased ^{10,26}.

Upon coating of particles by MAIC process, the process can modify surface property of HPs while their original size and shape is maintained almost, thus modifies their flowability ^{10, 22, 26}. However, number of GPs present on surface of the HPs has only a minor effect on flowability of the HPs, once cohesion force is reduced by presence of one or more GPs ^{10, 24}. Furthermore even with very discrete coating on surface of HPs, their flowability improves to significant level ^{10,25}.

connected to alternating current, refer Figure-3 ^{2-4,10,24}. The GPs and HPs are poured into the vessel followed by adding measured mass of magnetic particles ^{2,10}. Magnetic particles usually are of barium ferrite that is with polyurethane coating for preventing contamination of coated particles ^{3,10}. Presence of magnetic field, agitates magnetic particles that move frequently (oscillates) inside vessel thus fluidises the particle as in fluidised-bed system ^{4,10,25}. Agitated magnetic particle imparts energy to GPs and HPs thus causing their collisions (host-guest particles, host-host particles, host-GPs-vessel wall) ^{2,10}. Said collisions allow occurring of coating by way of impaction and/or peening of GPs onto HPs ¹⁰. Due to magnetic field the primary motion is spinning of the magnetic particles, which promotes de-agglomeration of GPs via-a-vis shearing and spreading of GPs onto surface of HPs ^{3,10,25}. However translational speed allows impaction of one particle onto some other, is also has significant effect in promoting coating ^{4,10}.

When primary GPs are in sub-micron range, the attraction forces (electrostatic, Van der Waals, etc) among them are relatively very high thus requires larger forces for their separation ^{10, 22}. HPs that are smaller can achieve higher velocities comparing to larger one from their collision with magnetic particles. This results in higher impaction forces; which is sufficient to break structure of agglomerated GPs ^{10, 24}. Researcher found that reduction in cohesion force for the coated particles is inversely pro-rata to particle size ratio of guest-to-host particles ^{10, 25}. This indicates smaller GPs provisioning larger reduction in their cohesive force ¹⁰.

HMC PROCESSES/ TECHNOLOGIES

Situations calls for HMC are elimination for use of aqua or non-aqua solvents, enhancing solubility and dissolution rate of poorly aqua-soluble drug, enhancing chemical stability of moisture sensitive drugs, and many more ²⁷⁻²⁹. An absence of solvent evaporation phase results strong and nonporous particles ^{2,3,27,30}.

In this process, as the name implies, melttable CoM, in the molten state, is applied onto substrate particle that solidifies upon cooling. The process uses melttable CoMs with low melting point, usually lipid or waxes ³⁰⁻³³. The process requirement is the melttable CoMs had to be heated to molten state for having their solution that then air-atomised and sprayed onto surface of moving solid substrate followed by

cooling of the product^{30, 32, 33}. Upon cooling, a continuous film forms on substrate that acts as moisture protection barrier coating or rate-controlling membrane for drug release^{4, 10}. Pan coater, spheronizer, spouted or fluid bed processors are required for HMC processes^{2-4, 10}.

As a process requirement, during application the coating fluid is required to be maintained at a constant temperature that cannot exceed 150 °C^{4, 32, 33}. Thus meltable materials having molten viscosity below 300 centipoises and melting points below 80 °C are generally suitable, as prior to spraying the molten CoMs are to be maintained at 40-60 °C above their melting point⁴. Ideally, meltable materials must have defined melting point or narrow range of melting point^{2, 3}.

Meltable materials are hydrophilic or water-soluble and hydrophobic or water-insoluble^{2, 3}. Change in consistency of molten droplets is achievable by inclusion of viscosity modifier into meltable matrix^{3, 4}. Viscosity modifier may be

meltable or non-meltable at processing temperature^{2, 4}. Typical melting range of various water-soluble and water insoluble binders be using in pharmaceutical formulation are provided with Table-2^{2, 3}.

Dry particles (like powders, pellets, granules) with mean particle size ranging between 100 -2000 µm can be subjected for HMC process using fluidised bed process where molten droplet size, temperature of outlet and inlet air, and fluidization air volume are well controlled^{4, 24}.

Lipidic meltable CoMs are highly compatible with ingredients like artificial sweeteners, flavouring agents, surfactants and many others^{4, 32, 33}. These processes are suitable for herbal and hygroscopic products^{2, 3}. Coated particles can be used in sachets, capsules, suspensions, and tablets. In flash melt and chewable tablet forms, plasticity along with resistance to fracture under pressure properties of the lipid coatings imparts interesting aspect of is these products²⁻⁴.

Table 2: Most commonly used CoMs and their melting point^{2, 3, 32, 33}.

Hydrophobic meltable materials	Melting point	Hydrophilic meltable materials	Melting point
Beeswax	62-65 °C	Gelucire® 50/13	44 - 50
Carnauba wax	47-50	Poloxamer 188	50.9
Cetyl palmitate	67-75	Polyethylene glycols (PEGs)	
Cottonseed oil	61-65	PEG 2000	42-53
Glycerol behenate	47-63	PEG 3000	48-63
Glycerol monostearate	48-57	PEG 6000	49-63
Glycerol palmitostearate	54-63	PEG 8000	54-63
Glycerol stearate	62-86	PEG 10000	57-64
Hydrogenated castor oil	58-72	PEG 20000	53-66
Microcrystalline wax	47-65		
Paraffin wax	46-69		
Partially hydrogenated palm oil	56-60		
Stearic acid	54-60		
Stearyl alcohol	57-61		

HMC Using Tablet Coating Pan

It is termed also as direct blending coating. The process involves application of CoM, in molten state, onto moving substrate, in a tablet coating pan that is continuously heated²⁻⁴. Cetyl alcohol and Gelucire® 50/13 are the suitable coating agents^{2-4, 24}.

Said technique is simple and does not call for sophisticated and complicated equipment². The process can be useful for wider range of substrates with diverse size and for coating in multiple layers^{3, 4}. The method comprises of follow steps^{2, 3}:

- (i) Melting of CoM²,
- (ii) Dissolving or dispersing drug in molten coating agent⁴,
- (iii) Applying molten solution or dispersion of CoM onto the moving substrate bed in a hot coating pan^{2, 3}.
- (iv) Through mixing of the molten coating agent and substrate particle⁴,

(v) Cooling of product with continued stirring of blend⁴, and

(vi) Congealing of coated substrate particles³.

Spray Congealing

A highly versatile technique of HMC process produces particles having diameter within range of 10-3000 µm^{2, 3}. The process involves spraying a hot-melt of wax, fatty acid, or glycerides into an air chamber below melting point of meltable materials or at cryogenic temperature. Granular particles are obtainable upon cooling^{2, 3}.

HMC using Fluid-Bed Processor

Interest for using fluid-bed processor in HMC has grown to significant level since 2001^{2, 3}. Powdered mixture of the meltable and the non-meltable materials fed onto the seeds (powder particle cores) in a fluid-bed processor^{24, 34-36}. The meltable materials can be added to the starting powder mixture can be in the form of either solid particles or molten liquid³⁷. Accordingly the procedure of the process basically

is ether melt-in procedure or spray-on procedure³⁸. Solid meltable binder melts during the process termed as melt-in procedure^{2, 34}. Process where molten liquid, optionally containing the dispersed drug, sprayed on is termed as spray-on procedure^{3, 35}. The melt-in procedure eliminates flow of molten liquid renders the procedure simpler for production comparing spray-on. Thus from industrial point of view, the melt-in procedure is favoured over the spray-on^{34, 36}.

The particle size and the viscosity of meltable materials and the temperatures of the inlet-air and the product endpoint significantly influence performance of HMC process^{24, 38}. Increased meltable material content increases coating thickness decreases dissolution rate of active^{38, 39}. The temperatures of the inlet-air and the product endpoint have more pronounced effect on parameters of coatings^{2, 3, 36, 39}.

In case of melt-in procedure, small meltable particles with sufficient viscous binding forces are obligatory for production of smooth and reproducible coat, thus should be keeping at an optimum value^{39, 40}. The particle size of meltable materials should be 1/6th or lower comparing the diameter of seeds and viscosity should be low³⁹. High-viscosity materials should be excluding for avoiding rough surface and non-uniform coating^{2, 3, 35, 40}.

Use of meltable materials of controlled properties makes the HMC process well controllable⁴¹. The melt pelletization and melt granulation processes desires meltable materials having a high viscosity and a reduced particle size^{42, 43}. High viscosity materials are desirous to improve mechanical strength of the coating but reduced particle size desirous to prevent rough surface of coating^{2, 3, 41}.

Solid Dispersion Hot-Melt Fluid-Bed Coating

A newer modified version of the HMC following fluid-bed process is solid dispersion based one, is often termed *Tumbling HMC*^{2, 24, 35, 44}. This process eliminates the spraying step thus does not calls for steam jackets, nozzles, and/or heating assembly³. Powder particles (termed non-pareils) and powder of PEG (as divided solid particle with size 1.41–3.36 mm) were fluidised together^{35, 36, 44}. The inlet air temperature is increased to melt the PEG thereby transferring them onto the non-pareils^{4, 44}. Then typical steps (like cooling and congealing) of HMC are followed^{4, 44}. Multiple coatings, as multiple layers, can be applied following this process^{4, 44}. For this, CoMs with diminishing rank order of their melting point is to be used to produce additive coating layers thus result multiple layered coatings^{4, 35}.

Turbo Jet Coating Process (Modified)

As an adaption to coat solid particles the process of Turbo Jet coating process is modified. The modified process involves suspending the solid particles in a spiral of ascending air^{2, 3, 24}. Said spiral air provides homogeneous distribution of individual particles²⁻⁴. The molten lipidic CoM is dispersed from bottom of tank and tangentially to particle flow²⁻⁴. The lipid crystallisation within nozzle expansion is however prevented using micro-environment surrounding nozzle outlet²⁻⁴. Said technique has ability to coat very fine particles, an advantage, as enable to suspend the particles within ascending air stream²⁻⁴.

Theta-composer

Theta-composer comprises of slowly rotating elliptical-vessel and fast rotating) elliptical rotor, that are rotating in opposite directions^{24, 45-49}. Rotor rotates anticlockwise (rotating between 900-1200 rpm) inside a clockwise rotating vessel (rotating between 30-40 rpm)^{4, 24}. Anticlockwise

rotation of rotor inside the clockwise rotating vessel forces powder mixture of HPs and GPs through small clearance between the rotor and the vessel thus subjects them for shearing and compressive stresses^{24, 45-48}. As rotor continue to move, clearance between rotor and vessel wall becomes large, there will be bulk mixing of HPs and GPs^{4, 24}. Through blending of HPs and GPs is to be done at a condition comprising of container speed at low and rotor speed at high^{4, 24}. At same time, application of strong shearing and compression forces accelerates precise blending & composite fabrication^{4, 24}.

Features and pros

Follows are the features and pros of theta-composer process⁴⁵⁻⁴⁸:

- Simple structure thus operation and maintenance is easier^{4, 24}.
- Slow rotational speed of the outside vessel promotes and favours bulk mixing^{4, 24}.
- High rotational speed of inside rotor confers high shear stress that is required for coating^{4, 24}.
- Elliptical shape of outside vessel and inside rotor is for stress and relaxation^{4, 24}.
- Rotation of vessel assists for getting fully homogenous powder composite without thermal deterioration^{4, 24}.
- Instant shearing and compression of particles minimises rise in temperature of materials^{4, 24}.
- Processing time is short^{4, 24}.
- Required rotational conditions can be selected that suits the material(s)^{4, 24}.
- Improves handling and increases flowability^{4, 24}.
- Suppress hygroscopicity^{4, 24}.

Mechanofusion

Underlying principle of the process is bringing forth a chemical-mechanical-reaction among two or more powder materials, to produce new material having differing properties^{24, 49-53}. The process employs a batch operated specifically designed device for fusing particle-to-particle at high compressive and shear forces thus resulting controlled particle shape^{4, 24}. The device comprises of outer vessel (rotating), inner piece (stationary), and scraper (stationary) as its key parts⁵⁰⁻⁵³.

Processing involves placing of aliquot amount of HPs and GPs into rotating vessel^{2-4, 24}. As vessel rotates at speed between 200 to 1600 rpm, powders are forced outwardly towards vessel⁵⁰⁻⁵³. Gap between inner stationary piece and rotating vessel is controlled; result is the powder particles passing thru gap are subjecting for intense compressive and shearing forces⁵⁰⁻⁵³. Combination of these forces acting on particles builds-up local temperature. The generated thermal energy is sufficient to fuse GPs onto surface of HPs⁵⁰⁻⁵³.

The size of gap between vessel wall and inner piece plays very important role as it controls thickness of the coating⁵⁰⁻⁵³. Gap between vessel wall and scraper also requires controlling^{2, 4, 24}.

Features and Pros

Features and pros of Mechanofusion process are as follows⁵⁰⁻⁵³.

- Produce composite particles with controlled particle shapes⁴.

- Eliminates need for pre-mixing of powder particles during processes of improving particle performance ²⁴.
- Control of process temperature can be doing using water cooled jacketed vessel ⁴.
- The compact design of devices eases coating process and enhances performance ²⁴.

HMC using spheronizer

The process involves use of laboratory scale spheronizer with slight modifications ^{54,55}. The process basis is feeding of dry CoMs along with substrate into spheronizer with smooth disk made up of stainless-steel ²⁻⁴. Edges of disk are leant at an angle of 45°, this facilitates tumbling movement of substrate and prevents loss of CoM ^{2,4}. An infrared lamp is used as source of heating, so for maintaining processing temperatures above the melting point of coating polymer ^{3,4}. Power supply of infrared lamp should be regulated and can be varied suitably to monitor and maintain process temperature ^{2,3}. Pipeline insulation is doing for preventing solidification of the molten CoMs, before occurrence of their final cooling on surface of substrate cores ^{3,4}. The process is advantageous as can use micronized polymers like Eudragit® E PO, an acrylic polymer, as CoM. Said coating process may be an alternate to aqueous or non-aqueous film coating process ^{4,8}.

The process calls for maintaining temperature of spheronizer disc below melting temperature of substrate but above *T_g* of meltable polymer, used. The *T_g* of meltable coating polymers are provided with Table-3 ^{4,8}.

Table 3: Some common meltable coating polymers and their *T_g* ^{4,8}.

Trade name	Polymer	T _g
Polyox WSR	Poly(ethylene oxide)	-67
Carbowax	Polyethylene glycol	-20
Kollidon	Poly vinyl pyrrolidone	168
PLGA	Poly (lactide-co-glycolide)	40-60
Elvanol	Polyvinyl alcohol	85
Ethocel	Ethyl cellulose	133
Klucel	Hydroxypropyl cellulose	130
Methocel	Hydroxypropyl methylcellulose	175
Eudragit® RS	Amino methacrylate copolymer	~ 65
Eudragit® RL	Amino methacrylate copolymer	58-68
Eudragit® E	Poly[(dimethylamino)ethyl methacrylate-co-methacrylic ester]	40-50
Eudragit® S	Poly(methyl methacrylate-co-methacrylic acid)	> 130

VAPOUR COATING OF POWDERS

It is a recently up-roused coating technology for solid dosage forms. It enables synthesising polymeric coating films with an orchestrated surface, topography, and functionalities with satisfactory coating uniformity. Vapour phase deposition is the principle used in methods for achieving vapour coating of powder ⁵⁷⁻⁶¹.

A powder or liquid can be dispersed by applying electrostatic field, a process referred as 'electro-dispersion' ^{2,4}. Electro-dispersion uses intense electric field to disperse a part of static-bed of powder or liquid into a stable cloud of

Spheroidization

Meltable materials used as CoMs this processes to coat core having diameter up to 500 μm ^{2,4}. The process suits utmost for having continuous and smooth coating of particle with improved flowability ^{3,4}. The powder blend passes rapidly through an area that is intensely heated; where the CoM melts, and flows onward to cold area; and yields a smooth surfaced particle as it cool-up ^{2,4}. As the meltable CoM and cores are in close proximity of each other, melting of CoM and pressurised flow of powder blend results coating of cores. Softening of thermoplastic cores, during the process, allows strong adherence of CoM to cores ^{3,4}.

Hybridizer

The hybridizer assembly (processing vessel) comprises of a six bladed very high speed rotating rotor, a stator, and a device made up of stainless steel or ceramic for powder re-circulation ^{24,49,56}. The re-circulation unit/ device continuously move particles in and out of processing chamber and against the rotor blades ^{2,4}. The powders (HPs and GPs) are placed in processing portion of vessel for subjecting them to forceful impactation & dispersion due to highly rotational speed of rotor ^{3,4}. A high impactation forces builds-up temperature and makes the particles for undergoing numerous collisions ^{2,4}. Powder collision result the breaking-up of the fine agglomerates and the powder coating, due to embedding or filming of GPs onto surface of HPs. The builds-up temperature is aiding in embedding or filming ^{3,4}.

fast moving particles (dispersed phase), and maintaining dynamic equilibrium in between the static phase and the dispersed phase ^{3,4}. Cloud density of the dispersed phase particles is dependent on numerous factors, including field strength and nature of powders ^{2,4}. Applied electric field also ensures that only uncoated particles are coated and avoids agglomeration of coated dispersed particles, as these repel each other due to possession of same charge ^{2,4}. Electro-deposition effect finds applicability in producing uniform, durable, and slow dissolving coatings of controlled thickness on individual particles ^{2,3}. This is achieved by generating a vapour of desired coating, typically semiconductor material

or a metal, and allowing vapour to permeate dispersed particles^{2,4}.

Basing on synthesis mechanisms follows major vapour phase deposition methods have applicability to pharmaceuticals²⁻⁴.

- a. CVD^{2,3}.
 - i. Plasma enhanced chemical vapour deposition.
 - ii. Initiated chemical vapour deposition.
- b. ALMD^{61,62}.

Vapour phase deposition reactions of CVD and ALMD are similar to as both utilises gaseous reagents for nurturing a film⁶⁰⁻⁶³. CVD is a single step process. While in ALMD, there is split-up of reactions into two surfaces half, it means a two-step reaction^{4,64}. This intends, it exposes substrate surface to one reagent only at a time^{4,61,62}. As a result of splitting the reaction into two steps, surface will be reacting sequentially with each reagent until complete surface is gets coated by a new atomic-layer^{4,62}. In simple words as the process starts, suppose reactant A is reacting with the surface functional groups present on particle⁴. Now, new surface functional groups are in place, and when this surface exposes to reactant B, the reactant B reacts with new functional groups⁴. The reaction is self-limiting thus reaction gets stopped when all totals of surface sites had been transformed back to original surface species^{4,62}. At this point, process can be repeating sequentially until wished film thickness is made achievable^{4,61}. The process results a monolayer (one complete cycle of A & B) with a film thickness of an order of 1 angstrom (0.1 nano-meters)^{4,62}.

Fluidised-bed chemical vapour coating: CVD on fluidised-bed of powder is one of most efficient technique to functionalise and to deposit on or coat individual powder particles from gaseous species by combining two processes⁶³. One process is deposition itself while other process aims to suspend particles in deposition zone, i.e., most often by upwardly flowing the gas through the powders⁶³. In general the method is transport limited. The process is followed for coating of titania⁴.

SCF based coating methods

SCFs are the highly compressed gasses. These possess several advantageous attributes of both gases and liquids⁶⁴⁻⁶⁶. Supercritical carbon dioxide (CO₂), nitrous oxide (N₂O), and alkanes (C₂ - C₄) are used as SCF, most widely²⁻⁴. However, for the pharmaceutical purposes, CO₂ is considered as an ideal SCF medium due to its comparatively low critical pressure of 72 bars and critical temperature of 31.1 °C, and follow advantages²⁻⁴.

- Low critical pressure and temperature value^{3,4}.
- Readily available^{2,4}.
- Cost-effective^{3,4}.
- Nontoxic, non-flammable^{2,4}.
- Highly pure^{3,4}.

Process basis

A minor change in pressure and/or temperature causes significant change in SCF density and rapid change in their solvent power, near their critical point⁶⁴⁻⁶⁶. Rapid expansion vis-à-vis rapid supersaturation translates into a rapid change in the density and solvent power of the SCF and therefore into rapid crystallization rates which result in precipitation of solute^{3,4}. Alternately rapid reduction in the

solvent power of the SCF without any substantial change in pressure consists of contacting the SCF solution with an inert gas like nitrogen or helium in which the CoM is insoluble^{2,4}. Rapid mixing is of inert gas with the SCF decreases solvent power of SCF and CoM to precipitate^{2,3}.

SCFs based particle coating methods that used most widely are follows^{3,4}:

- a. RESF method⁶⁷.
- b. GAS process⁶⁸.
- c. SCF anti-solvent method⁶⁷.
- d. GSS method^{67,69,70}.

RESF method

Rapid expansion of the supercritical solution is the underlying principle for having particle coating by polymer encapsulation⁶⁴⁻⁶⁷. The rapid expansion vis-à-vis rapid supersaturation translates into rapid change in the density and solvent power of the fluid and therefore into rapid crystallization rates result coating⁶⁴⁻⁶⁶. The process basis is using SCF for preparing solution of CoMs followed by its release at atmospheric pressure thru small nozzle(s)⁶⁴⁻⁶⁶.

Limitations

- Poor solubility of most CoMs in SCF^{2,4}.
- Active core to be insoluble is the basic requirement^{3,4}.
- Calls for necessary investment for having high-pressure processing equipments^{2,4}.

In this process CoM is solubilised in SCF under high pressure in a vessel^{3,4}. A dispersion of active(s) in resulting solution is prepared by dispersing the active(s)^{2,4}. The resultant suspension is maintained at high pressure which upon release thru a small nozzle, at atmospheric pressure, rapidly expands, thus reduces solvent power of the SCF^{3,4}. The sudden pressure drop causes desolvation of CoM thus gets precipitated onto particles of dispersed drug(s) in medium of SCF and forms a layer of coating on the dispersed drug particles^{2,4}.

CoMs having applicability were fatty acids, fatty alcohols, and lipids; lipids (viz. mono-, di-, & tri-glycerides of fatty acids) are used mainly, while combination of these CoMs with other lipids may be used^{3,4}.

Most of CoMs, including polymers, possesses very low solubility in SCFs (<1 % w/w) except for polymers with low cohesive force densities and fractions with low molecular weight^{2,4}. In these instances, co-solvents (acetone and/or methanol) are used for increasing their solubility in the SCFs^{3,4}. Further, in some instances non-solvents can be using, this increases solubility of CoMs in SCFs while don't dissolve them at the atmospheric pressure^{2,4}.

For having successful coating, ideally the SCF should dissolve the CoM only while leaving core completely undissolved^{3,4}.

GAS process

Here rapid reduction in the solvent power of the SCF without any substantial change in pressure is achieved by interacting solution of solutes (drug and CoM) in SCF with an inert gas like nitrogen or helium in which the solutes are insoluble^{2,68}. The inert gas, which acts as an antisolvent for solutes, may be kept at pressure par to that of solute solution in SCF^{3,4}. Design of the process is for dealing solutes (active and CoMs) that are soluble in SCF but are insoluble in inert gas^{2,4}. Rapid mixing is of inert gas with

SCF decreases solvent power of SCF and causes solute to precipitate^{2,3}.

Here the solution of CoM and active(s) in SCF maintained at high pressure, in a vessel^{2,4}. Then the inert gas, an antisolvent for solutes, is poured into the vessel^{2,3}. This results extraction of SCF from the solution causing super saturation to such extent that precipitation of solute occurs^{3,4}.

SCF anti-solvent method

Process has synonym in literature as '*Aerosol solvent extraction systems*' while variation thereof has been disclosed as '*Solution-enhanced dispersion by supercritical fluids*'^{66,67}. A process designed for the solutes (active and CoMs) that are soluble in organic solvent but are insoluble in SCF and solution of SCF and volatile organic solvent whilst organic solvent be miscible with SCF^{2,3}. It is suitable for processing material that has little solubility in SCF of choice and thermolabile substances^{2,4}. Submicron particles can be coated with this method but unable to coat aqua soluble materials^{3,4}. A batch process is limited in its ability to process large quantities of material^{2,3}.

Here the SCF is used as an antisolvent to process a SCF-insoluble solute, from a pre-mixed batch of an organic solution of the solute, involving addition of SCF into the organic solution^{3,4}. Addition of the SCF causes its concentration in organic solution to increase and solution to expand^{2,4}. Solute precipitation takes place as the solution becomes supersaturated^{2,3}.

Said process involves continuously adding the solution of solute in volatile organic solvent to continuously flowing SCF (antisolvent for the solute)^{3,4}. Organic solution rapidly mixes and dissolves in SCF forming a homogeneous high-pressure fluid mixture^{2,4}. Since solute is considerably insoluble in SCF, and volatile organic solvent and SCF are miscible, this results in precipitation of solutes in the high pressure vessel^{3,4}. The SCF-organic solvent mixture is passed through a micro-filter and then expanded into a low pressure vessel where the SCF separates from the volatile organic solvent^{2,3}.

GSS method

Here mixing of core particles and CoMs in SCF is done, at high pressure. SCF penetrates CoM causing their swelling^{67,69,70}. Resultant mixture is then heated above the T_g of polymer to liquefy coating polymer^{2,4}. Then, when pressure is released, the CoM gets deposited onto active cores. The process does not require that the active core and the CoMs soluble in SCF^{3,4}.

CONCLUSION

The sequential steps of DPC (powder application, coalescence, and sintering) are influenced by coating formulation and process. In DPC processes, appropriate particle size of materials is essential for ensuring and reproducing uniformity of coating. A general recommendation is CoM's diameter be less than 1 % that of the substrate. This permits application of CoM onto substrate surface to an acceptable degree of uniformity, improve film adhesion and appearance, and decrease processing time. During coating process, heating of substrates are often done above the T_g of the CoMs for causing softening of layering materials to aid its adherence to substrate.

Some of DPC process relies on mechanical compaction occurring naturally during the process. Said mechanical compaction facilitates adhesion and coalescence. Under this

circumstances, the stresses on coating layer results consolidation of substrate bed and spreading of coating layer across interface driven by deformation. In case of elastic materials, deformation of material is reversible bearing for poor contact across the surface. While in case of coatings exhibiting plastic behaviour, deformation is permanent (irreversible) and mechanical compaction contributes to greater adhesion of surface layer. This improved adhesion is due to larger surface area for contact between substrate and coating, as well as possible mechanical interlocking of the materials.

Modification in the spreading and adhesion behaviour can also be achieved through application of sub-coat to substrate. Sub-coating involves layering of new material, corresponding to 2-3 % w/w weight gain of substrate core, which can facilitate adhesion/ adherence of the powder coat by changing interfacial energy.

Literature reports on extensive use of low melting point hydrophilic polymers like PEG 3350 are there while available also report on use of other materials having amphiphilic and hydrophobic properties.

Intentional selection of sub-coat material that can remain in molten (partially) state at the processing temperatures promotes further adhesion with the coating layer. Here molten priming layer promote adhesion of powdery coating particles through forming liquid bridge with the substrate surface. Interfacial interactions amongst the polymer particles (to be layered) and substrate surface are rather complex which depends on adhesion, interfacial tension, and wetting.

Dry coating technologies possess enormous advantages but inferior uniformity of coating film is biggest challenge that hinders their application and commercialisation, the main goal requires addressing.

ACKNOWLEDGEMENT AND CONFLICT OF INTEREST

No conflicts of interest had been published in relation to this paper. However for continual support and encouragement author will remain indebted to the administration and the staffs of Jeypore College of Pharmacy, Jeypore, Koraput, Odisha, India.

REFERENCES

1. Saikh MAA, Aqueous film coating the current trend. *Journal of Drug Delivery and Therapeutics*, 2021; 11(4-S):212-224. DOI: <https://dx.doi.org/10.22270/jddt.v11i4-S.4911>.
2. Saikh MAA. *Pharmaceutical's Granulation*. Germany: LAP Lambert Academic Publishing; 2016.
3. Saikh MAA. *Pharmaceutical's Coating*. Germany: LAP Lambert Academic Publishing; 2015.
4. Chavda VP, Soniwala MM, Chavda JR. Particle coating: From conventional to advanced. *International Journal of Pharmaceutical and Medicinal Research*, 2013; 1:1-17.
5. Singhai NJ, Rawal A, Maurya R, Suman R. Design and characterization of dual drug loaded microspheres for colon drug targeting. *Journal of Drug Delivery and Therapeutics*, 2019; 9(3-S):12-22. DOI: <https://dx.doi.org/10.22270/jddt.v9i3-s.2923>.
6. Gaware RU, Tambe ST, Dhobale SM, Jadhav SL. Formulation and in-vitro evaluation of theophylline sustained release tablet. *Journal of Drug Delivery and Therapeutics*, 2019; 9(1-S):48-51. DOI: <https://dx.doi.org/10.22270/jddt.v9i1-s.2252>.
7. Divya B, Sreekanth J, Satyavati D. Development of extended release formulations of llaprazole tablets. *Journal of Drug*

- Delivery and Therapeutics, 2019; 9(3):8-12. DOI: <https://dx.doi.org/10.22270/jddt.v9i3.2811>.
8. Yang Q, Yuan F, Xu L, Yan Q, Yang Y, Wu D, Guo F, Yang G. An update of moisture barrier coating for drug delivery. *Pharmaceutics*, 2019; 11(9):436. DOI: <https://dx.doi.org/10.3390/pharmaceutics11090436>.
 9. Pundir K, Parashar B. The innovations in tablet coating: A review. *International Educational Applied Research Journal*, 2019; 3(6):18-23.
 10. Ahmed SAN, Patil SR, Khan MKS, Khan MS. Tablet coating techniques: Concept and recent trends. *International Journal of Pharmaceutical Sciences Review and Research*, 2021; 66(1):43-53.
 11. Yang Q, Ma Y, Zhu J. Dry powder coated osmotic drug delivery system. *European Journal of Pharmaceutical Sciences*, 2018; 111:383-392. DOI: <https://dx.doi.org/10.1016/j.ejps.2017.10.001>.
 12. Foppoli AA, Maroni A, Cerea M, Zema L, Gazzaniga A. Dry coating of solid dosage forms: An overview of processes and applications. *Drug Development and Industrial Pharmacy*, 2017; 43(12):1919-1931.
 13. Yang Q, Ma Y, Zhu J, Chow K, Shi K. An update on electrostatic powder coating for pharmaceuticals. *Particuology*, 2017; 31:1-7. DOI: <https://dx.doi.org/10.1016/j.partic.2016.10.001>.
 14. Yang Q, Ma Y, Shi K, Yang G, Zhu J. Electrostatic coated controlled porosity osmotic pump with ultrafine powders. *Powder Technology*, 2018; 333:71-77. DOI: <https://dx.doi.org/10.1016/j.powtec.2018.04.009>.
 15. Prasad LK, McGinity JW, Williams RO 3rd. Electrostatic powder coating: Principles and pharmaceutical applications. *International Journal of Pharmaceutics*, 2016; 505(1-2):289-302. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2016.04.016>.
 16. Yang Y, Shen L, Yuan F, Fu H, Shan W. Preparation of sustained release capsules by electrostatic dry powder coating, using traditional dip coating as reference. *International Journal of Pharmaceutics*, 2018; 543(1-2):345-351. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2018.03.047>.
 17. Qiao M, Luo Y, Zhang L, Ma Y, Stephenson TS, Zhu J. Sustained release coating of tablets with Eudragit® RS/RL using a novel electrostatic dry powder coating process. *International Journal of Pharmaceutics*, 2010; 399(1-2):37-43. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2010.07.047>.
 18. Qiao M, Zhang L, Ma Y, Zhu J, Xiao W. A novel electrostatic dry coating process for enteric coating of tablets with Eudragit® L 100-55. *European Journal of Pharmaceutics and Biopharmaceutics*, 2013; 83(2):293-300. DOI: <https://dx.doi.org/10.1016/j.ejpb.2012.10.006>.
 19. Yang Q, Ma Y, Zhu J. Applying a novel electrostatic dry powder coating technology to pellets. *European Journal of Pharmaceutics and Biopharmaceutics*, 2015; 97(PtA):118-124. DOI: <https://dx.doi.org/10.1016/j.ejpb.2015.10.006>.
 20. Yang Q, Ma Y, Zhu J. Sustained drug release from electrostatic powder coated tablets with ultrafine Ethylcellulose powders. *Advanced Powder Technology*, 2016; 27(5):2145-2152. DOI: <https://dx.doi.org/10.1016/j.apt.2016.07.027>.
 21. Barletta T M, Tagliaferri V. Electrostatic fluidized bed deposition of a high performance polymeric powder on metallic substrates. *Surface & Coatings Technology*, 2006; 200:4282-4290.
 22. Ramlakhan M, Yu Wu C, Watano S, Dave RN, Pfeffer R. Dry particle coating using magnetically assisted impaction coating: Modification of surface properties and optimization of system and operating parameters. *Powder Technology*, 2000; 112(1-2):137-148. DOI: [https://dx.doi.org/10.1016/S0032-5910\(99\)00314-9](https://dx.doi.org/10.1016/S0032-5910(99)00314-9).
 23. Singh RK, Ata A, Fitz-Gerald J, Rabinovich Y, Hendrickson W. Dry coating method using magnetically assisted impaction in a randomly turbulent fluidized bed. *Kona Powder and Particle Journal*, 1997; 15:121-131. DOI: <https://dx.doi.org/10.14356/kona.1997016>.
 24. Gera M, Saharan VA, Kataria M, Kukkar V. Mechanical methods for dry particle coating processes and their applications in drug delivery and development. *Recent Patents on Drug Delivery & Formulation*, 2010; 4(1):58-81. DOI: <https://dx.doi.org/10.2174/187221110789957200>.
 25. Jallo LJ, Dave RN. Explaining electrostatic charging and flow of surface-modified Acetaminophen powders as a function of relative humidity through surface energetics. *Journal of Pharmaceutical Sciences*, 2015; 104(7):2225-2232. DOI: <https://dx.doi.org/10.1002/jps.24479>.
 26. Jallo LJ, Ghoroi C, Gurumurthy L, Patel U, Davé RN. Improvement of flow and bulk density of pharmaceutical powders using surface modification. *International Journal of Pharmaceutics*, 2012; 423(2):213-225. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2011.12.012>.
 27. Stocker E, Becker K, Hate S, Hohl R, Schiemenz W, Sacher S, Zimmer A, Salar-Behzadi S. Application of ICH Q9 quality risk management tools for advanced development of hot melt coated multiparticulate systems. *Journal of Pharmaceutical Sciences*, 2017; 106(1):278-290. DOI: <https://dx.doi.org/10.1016/j.xphs.2016.09.025>.
 28. Zier KI, Schultze W, Leopold CS. Combination of a hot-melt subcoating and an enteric coating for moisture protection of hygroscopic *Sennae fructus* tablets. *Pharmaceutical Development and Technology*, 2019; 24(10):1210-1217. DOI: <https://dx.doi.org/10.1080/10837450.2019.1648509>.
 29. Wang X, Wang P, Huang C, Lin X, Gong H, He H, Cai C. Hot-melt sub- and outer coating combined with enteric aqueous coating to improve the stability of aspirin tablets. *Asian Journal of Pharmaceutical Sciences*, 2017; 12(3):266-278. DOI: <https://dx.doi.org/10.1016/j.ajps.2016.11.003>.
 30. Bannow J, Koren L, Salar-Behzadi S, Löbmann K, Zimmer A, Rades T. Hot melt coating of amorphous Carvedilol. *Pharmaceutics*, 2020; 12(6):519. DOI: <https://dx.doi.org/10.3390/pharmaceutics12060519>.
 31. Jannin V, Cuppok Y. Hot-melt coating with lipid excipients. *International Journal of Pharmaceutics*, 2013; 457(2):480-487. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2012.10.026>.
 32. Salar-Behzadi S, Corzo C, Gomes Lopes D, Meindl C, Lochmann D, Reyer S. Novel approach for overcoming the stability challenges of lipid-based excipients. Part 2: Application of polyglycerol esters of fatty acids as hot melt coating excipients. *European Journal of Pharmaceutics and Biopharmaceutics*, 2020; 148:107-117. DOI: <https://dx.doi.org/10.1016/j.ejpb.2020.01.009>.
 33. Salar-Behzadi S, Corzo C, Schaden L, Laggner P, Zimmer A. Correlation between the solid state of lipid coating and release profile of API from hot melt coated microcapsules. *International Journal of Pharmaceutics*, 2019; 565:569-578. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2019.05.036>.
 34. Guimarães TF, Comelli ACC, Tacón LA, Cunha TA, Marreto RN, Freitas LAP. Fluidized bed hot melt granulation with hydrophilic materials improves Enalapril maleate stability. *AAPS PharmSciTech*, 2017; 18(4):1302-1310. DOI: <https://dx.doi.org/10.1208/s12249-016-0593-0>.
 35. Schertel S, Salar-Behzadi S, Karrer J, Laggner P, Zimmer A. Impact of Polysorbate 65 on Tripalmitin crystal growth and release stability of hot melt coated multiparticulate systems. *International Journal of Pharmaceutics*, 2021; 607:120970. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2021.120970>.
 36. Schertel S, Salar-Behzadi S, Zimmer A. Impact of surface properties of core material on the stability of hot melt-coated multiparticulate systems. *Pharmaceutics*, 2021; 13(3):366. DOI: <https://dx.doi.org/10.3390/pharmaceutics13030366>.
 37. Lopes DG, Salar-Behzadi S, Zimmer A. Designing optimal formulations for hot-melt coating. *International Journal of*

- Pharmaceutics, 2017; 533(2):357-363. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2017.08.086>.
38. Lopes DG, Garsuch V, Becker K, Paudel A, Stehr M, Zimmer A, Salar-Behzadi S. Improving the granule strength of roller-compacted ibuprofen sodium for hot-melt coating processing. *International Journal of Pharmaceutics*, 2016; 510(1):285-295. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2016.06.049>.
39. Hohl R, Scheibelhofer O, Stocker E, Behzadi SS, Haack D, Koch K, Kerschhaggl P, Lochmann D, Sacher S, Zimmer A. Monitoring of a hot melt coating process via a novel multipoint near-infrared spectrometer. *AAPS PharmSciTech*, 2017; 18(1):182-193. DOI: <https://dx.doi.org/10.1208/s12249-016-0504-4>.
40. Yeung CW, Rein H. Determination of surface energies of hot-melt extruded sugar-starch pellets. *Pharmaceutical Development and Technology*, 2018; 23(2):198-206. DOI: <https://dx.doi.org/10.1080/10837450.2017.1395886>.
41. Milanovic A, Aleksic I, Ibric S, Parojcic J, Cvijic S. Tableting of hot-melt coated Paracetamol granules: Material tableting properties and quality characteristics of the obtained tablets. *European Journal of Pharmaceutical Sciences*, 2020; 142:105121. DOI: <https://dx.doi.org/10.1016/j.ejps.2019.105121>.
42. Jedinger N, Schrank S, Fischer JM, Breinhalter K, Khinast J, Roblegg E. Development of an abuse- and alcohol-resistant formulation based on hot-melt extrusion and film coating. *AAPS PharmSciTech*, 2016; 17(1):68-77. DOI: <https://dx.doi.org/10.1208/s12249-015-0373-2>.
43. Yang Y, Shen L, Li J, Shan WG. Preparation and evaluation of Metoprolol tartrate sustained-release pellets using hot melt extrusion combined with hot melt coating. *Drug Development and Industrial Pharmacy*, 2017; 43(6):939-946. DOI: <https://dx.doi.org/10.1080/03639045.2017.1287715>.
44. Liu Y, Doddi J, Zheng Y, Ho V, Pheil M, Shi Y. Transmission raman spectroscopic quantification of active pharmaceutical ingredient in coated tablets of hot-melt extruded amorphous solid dispersion. *Applied Spectroscopy*, 2020; 74(1):108-115. DOI: <https://dx.doi.org/10.1177/0003702819884994>.
45. Shibata Y, Fujii M, Sugamura Y, Yoshikawa R, Fujimoto S, Nakanishi S, Motosugi Y, Koizumi N, Yamada M, Ouchi K, Watanabe Y. The preparation of a solid dispersion powder of Indomethacin with Crospovidone using a twin-screw extruder or kneader. *International Journal of Pharmaceutics*, 2009; 365(1-2):53-60. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2008.08.023>.
46. Iida K, Hayakawa Y, Okamoto H, Danjo K, Luenberger H. Influence of storage humidity on the in vitro inhalation properties of Salbutamol sulfate dry powder with surface covered lactose carrier. *Chemical and Pharmaceutical Bulletin (Tokyo)*, 2004; 52(4):444-446. DOI: <https://dx.doi.org/10.1248/cpb.52.444>.
47. Iida K, Inagaki Y, Todo H, Okamoto H, Danjo K, Luenberger H. Effects of surface processing of lactose carrier particles on dry powder inhalation properties of Salbutamol sulfate. *Chemical and Pharmaceutical Bulletin (Tokyo)*, 2004; 52(8):938-942. DOI: <https://dx.doi.org/10.1248/cpb.52.938>.
48. Iida K, Hayakawa Y, Okamoto H, Danjo K, Luenberger H. Effect of surface covering of lactose carrier particles on dry powder inhalation properties of Salbutamol sulfate. *Chemical and Pharmaceutical Bulletin (Tokyo)*, 2003; 51(12):1455-1457. DOI: <https://dx.doi.org/10.1248/cpb.51.1455>.
49. Quinlan L, Morton DAV, Zhou Q. Particle engineering via mechanical dry coating in the design of pharmaceutical solid dosage forms. *Current Pharmaceutical Design*, 2015; Article Number 21(999). DOI: <https://dx.doi.org/10.2174/1381612821666151008151001>.
50. Jeon IS, Lee MH, Choi HH, Lee S, Chon JW, Chung DJ, Park JH, Jho JY. Mechanical properties and bioactivity of polyetheretherketone/hydroxyapatite/carbon fiber composite prepared by the mechanofusion process. *Polymers (Basel)*, 2021; 13(12):1978. DOI: <https://dx.doi.org/10.3390/polym13121978>.
51. Koskela J, Morton DAV, Stewart PJ, Juppo AM, Lakio S. The effect of mechanical dry coating with Magnesium stearate on flowability and compactibility of plastically deforming microcrystalline cellulose powders. *International Journal of Pharmaceutics*, 2018; 537(1-2):64-72. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2017.11.068>.
52. Bungert N, Kobler M, Scherließ R. In-depth comparison of dry particle coating processes used in dpi particle engineering. *Pharmaceutics*, 2021; 13(4):580. DOI: <https://dx.doi.org/10.3390/pharmaceutics13040580>.
53. Matsumoto A, Ono A, Murao S, Murakami M. Microparticles for sustained release of water-soluble drug based on a containment, dry coating technology. *Drug Discoveries & Therapeutics*, 2018; 12(6):347-354. DOI: <https://dx.doi.org/10.5582/ddt.2018.01082>.
54. Cerea M, Zheng W, Young CR, McGinity JW. A novel powder coating process for attaining taste masking and moisture protective films applied to tablets. *International Journal of Pharmaceutics*, 2004; 279(1-2):127-139. DOI: <https://dx.doi.org/10.1016/j.ijpharm.2004.04.015>.
55. Sauer D, Zheng W, Coots LB, McGinity JW. Influence of processing parameters and formulation factors on the drug release from tablets powder-coated with Eudragit L 100-55. *European Journal of Pharmaceutics and Biopharmaceutics*, 2007; 67(2):464-475. DOI: <https://dx.doi.org/10.1016/j.ejpb.2007.02.021>.
56. otles S, Lecoq O, Dodds JA. Dry particle high-impact coating of biopowders: coating strength. *Particulate Science and Technology*, 2009; 27(4):352-361. DOI: <https://dx.doi.org/10.1080/02726350902993987>.
57. Christian P, Ehmann HM, Coclite AM, Werzer O. Polymer encapsulation of an amorphous pharmaceutical by initiated chemical vapor deposition for enhanced stability. *ACS Applied Materials & Interfaces*, 2016; 8(33):21177-21184. DOI: <https://dx.doi.org/10.1021/acsami.6b06015>.
58. Christian P, Ehmann HM, Werzer O, Coclite AM. Wrinkle formation in a polymeric drug coating deposited via initiated chemical vapor deposition. *Soft Matter*, 2016; 12(47):9501-9508. DOI: <https://dx.doi.org/10.1039/c6sm01919f>.
59. Perrotta A, Werzer O, Coclite AM. Strategies for drug encapsulation and controlled delivery based on vapor-phase deposited thin films. *Advanced Engineering Materials*, 2017; 20:1700639. DOI: <https://dx.doi.org/10.1002/adem.201700639>.
60. Tylinksi M, Smith RS, Kay BD. Morphology of vapor-deposited acetonitrile films. *Journal of Physical Chemistry A*, 2020; 124(30):6237-6245. DOI: <https://dx.doi.org/10.1021/acs.jpca.0c03650>.
61. Wack S, Lunca Popa P, Adjeroud N, Vergne C, Leturcq R. Two-Step approach for conformal chemical vapor-phase deposition of ultra-thin conductive silver films. *ACS Applied Materials & Interfaces*, 2020; 12(32):36329-36338. DOI: <https://dx.doi.org/10.1021/acsami.0c08606>.
62. Li H, Gao Y, Shao Y, Su Y, Wang X. Vapor-Phase atomic layer deposition of CO9S8 and its application for supercapacitors. *Nano Letters*, 2015; 15(10):6689-6695. DOI: <https://dx.doi.org/10.1021/acs.nanolett.5b02508>.
63. Santino LM, Hwang E, Diao Y, Lu Y, Wang H, Jiang Q, Singamaneni S, D'Arcy JM. Condensing vapor phase polymerization (cvpp) of electrochemically capacitive and stable polypyrrole microtubes. *ACS Applied Materials & Interfaces*, 2017; 9(47):41496-41504. DOI: <https://dx.doi.org/10.1021/acsami.7b13874>.
64. Soh SH, Lee LY. Microencapsulation and nanoencapsulation using supercritical fluid (SCF) techniques. *Pharmaceutics*, 2019; 11(1):21. DOI: <https://dx.doi.org/10.3390/pharmaceutics11010021>.

65. Trivedi V, Bhomia R, Mitchell JC. Myristic acid coated protein immobilised mesoporous silica particles as pH induced oral delivery system for the delivery of biomolecules. *Pharmaceuticals (Basel)*, 2019; 12(4):153. DOI: <https://dx.doi.org/10.3390/ph12040153>.
66. Chen LF, Xu PY, Fu CP, Kankala RK, Chen AZ, Wang SB. Fabrication of supercritical antisolvent (SAS) process-assisted Fisetin-encapsulated poly (vinyl pyrrolidone) (PVP) nanocomposites for improved anticancer therapy. *Nanomaterials (Basel)*, 2020; 10(2):322. DOI: <https://dx.doi.org/10.3390/nano10020322>.
67. Sheth P, Sandhu H, Singhal D, Malick W, Shah N, Kislalioglu MS. Nanoparticles in the pharmaceutical industry and the use of supercritical fluid technologies for nanoparticle production. *Current Drug Delivery*, 2012; 9(3):269-284. DOI: <https://dx.doi.org/10.2174/156720112800389052>.
68. Amania M, Saadati N, Navid A, Majda Y. Utilization of supercritical CO₂ gas antisolvent (GAS) for production of Capecitabine nanoparticles as anti-cancer drug: Analysis and optimization of the process conditions. *Journal of CO₂ Utilization*, 2021; 46:101465. DOI: <https://dx.doi.org/10.1016/j.jcou.2021.101465>.
69. Silva JM, Akkache S, Araújo AC, Masmoudi Y, Reis RL, Badens E, Duarte ARC. Development of innovative medical devices by dispersing fatty acid eutectic blend on gauzes using supercritical particle generation processes. *Materials Science & Engineering. C, Materials for Biological Applications*, 2019; 99:599-610. DOI: <https://dx.doi.org/10.1016/j.msec.2019.02.012>.
70. Perinelli DR, Cespi M, Bonacucina G, Naylor A, Whitaker M, Lam JK, Howdle SM, Casettari L, Palmieri GF. PEGylated biodegradable polyesters for PGSS microparticles formulation: Processability, physical and release properties. *Current Drug Delivery*, 2016; 13(5):673-81. DOI: <https://dx.doi.org/10.2174/1567201813666151207111034>.